

Bioengineering 280A
Principles of Biomedical Imaging

Fall Quarter 2004
X-Rays/CT Lecture 1

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Topics

- X-Rays
- Computed Tomography
- Direct Inverse and Iterative Inverse
- Backprojection
- Projection Theorem
- Filtered Backprojection

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EM spectrum

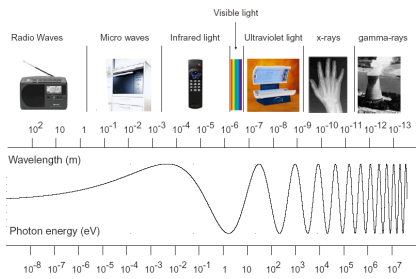
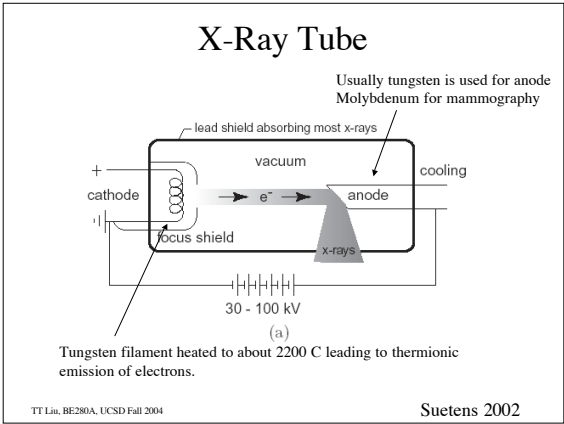
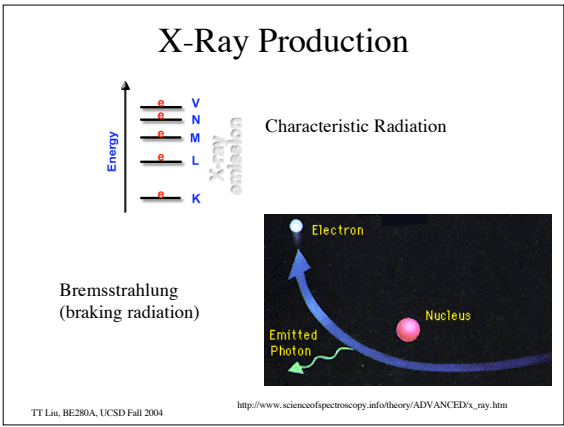


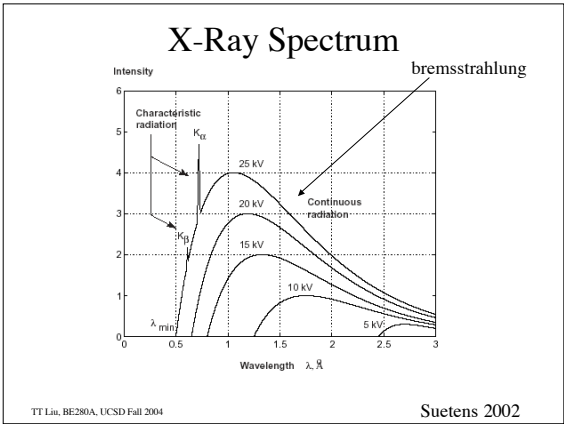
Figure 4.1: The electromagnetic spectrum.

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Interaction with Matter

Typical energy range for diagnostic x-rays is below 200 keV. The two most important types of interaction are photoelectric absorption and Compton scattering.

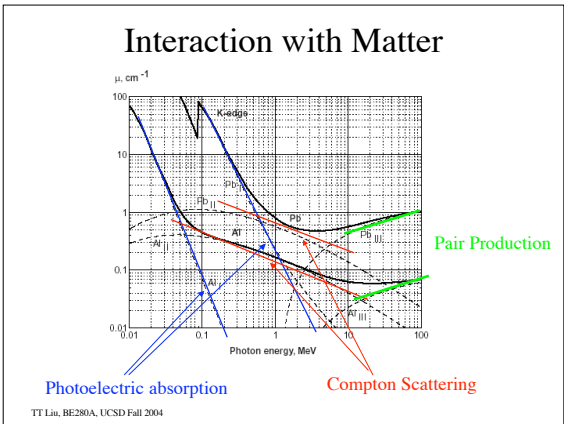
(a) X-ray Photon
(b) Photoelectron
(c) Ejected Photon

(a) X-ray Photon
(b) Ejected Electron
(c) Modified Photon

Photoelectric effect dominates at low x-ray energies and high atomic numbers.

Compton scattering dominates at high x-ray energies and low atomic numbers, not much contrast

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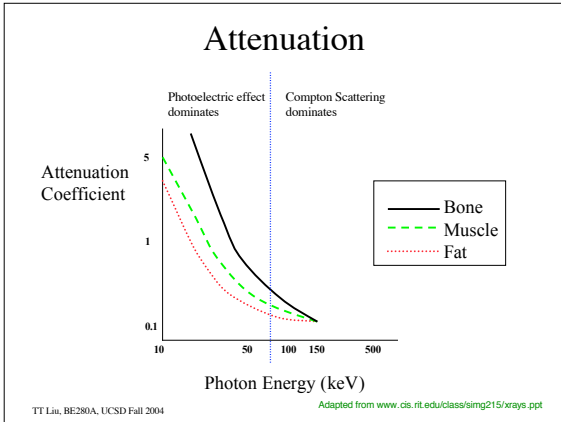
Attenuation

For single-energy x-rays passing through a homogenous object:

$$I_{out} = I_{in} \exp(-\mu d)$$

Linear attenuation coefficient

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Half Value Layer

X-ray energy (keV)	HVL, muscle (cm)	HVL Bone (cm)
30	1.8	0.4
50	3.0	1.2
100	3.9	2.3
150	4.5	2.8

In chest radiography, about 90% of x-rays are absorbed by body. Average energy from a tungsten source is 68 keV. However, many lower energy beams are absorbed by tissue, so average energy is higher. This is referred to as beam-hardening, and reduces the contrast.

Values from Webb 2003

Attenuation

For an inhomogenous object:

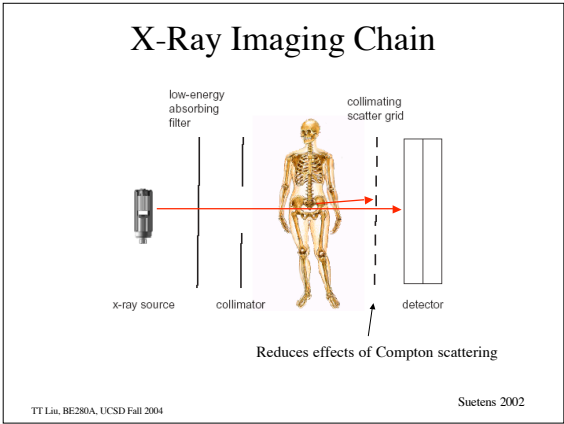
$$I_{out} = I_{in} \exp\left(-\int_{x_{in}}^{x_{out}} \mu(x) dx\right)$$

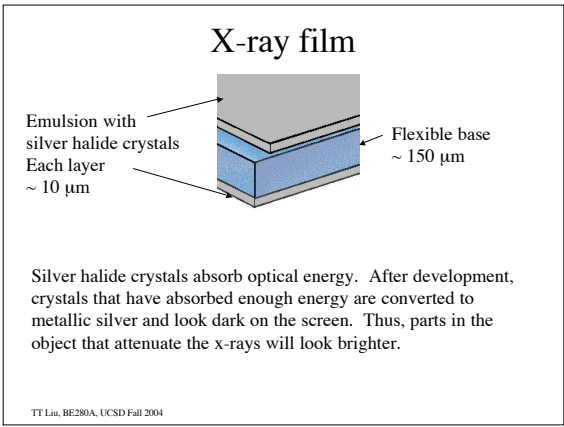
Integrating over energies

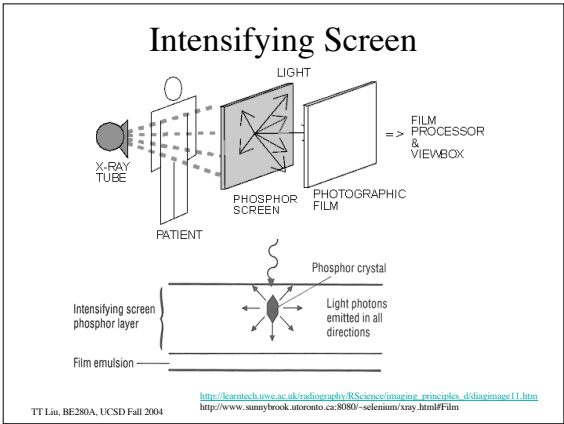
$$I_{out} = \int_0^\infty \sigma(E) \exp\left(-\int_{x_{in}}^{x_{out}} \mu(E, x) dx\right) dE$$

↙
Intensity distribution of beam

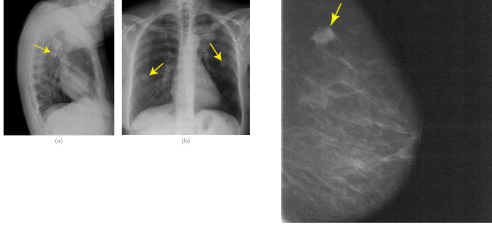
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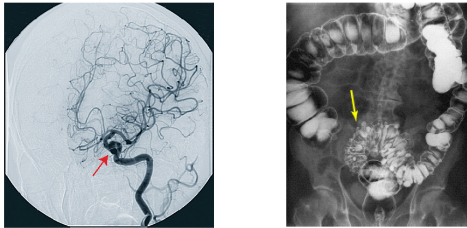
X-Ray Examples



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X-Ray w/ Contrast Agents



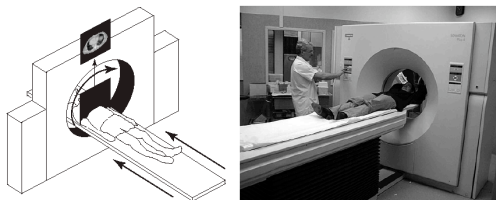
Angiogram using an iodine-based contrast agent.
K-edge of iodine is 33.2 keV

Barium Sulfate
K-edge of Barium is 37.4 keV

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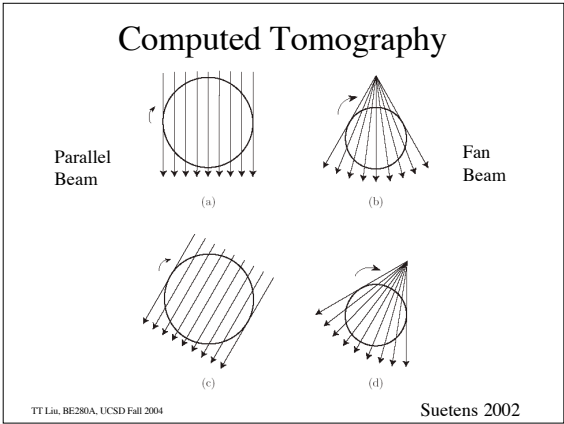
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Computed Tomography



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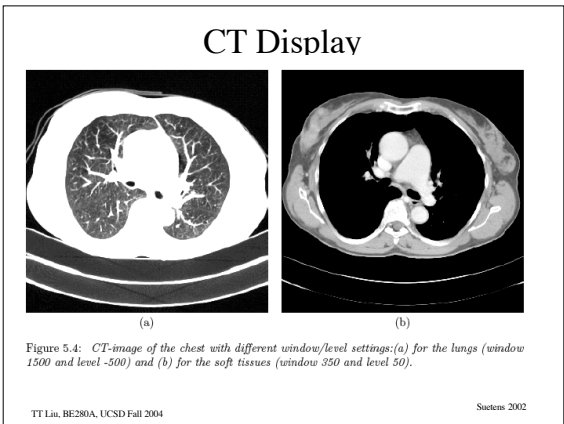
CT Number

$$CT_number = \frac{\mu - \mu_{water}}{\mu_{water}} \times 1000$$

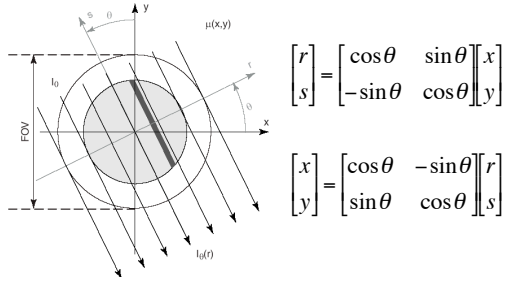
Measured in Hounsfield Units (HU)

Air: -1000 HU
 Soft Tissue: -100 to 60 HU
 Cortical Bones: 250 to 1000 HU

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Projections



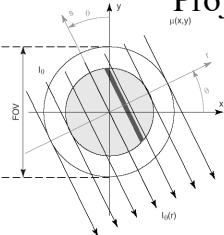
$$\begin{bmatrix} r \\ s \end{bmatrix} = \begin{bmatrix} \cos \theta & \sin \theta \\ -\sin \theta & \cos \theta \end{bmatrix} \begin{bmatrix} x \\ y \end{bmatrix}$$

$$\begin{bmatrix} x \\ y \end{bmatrix} = \begin{bmatrix} \cos \theta & -\sin \theta \\ \sin \theta & \cos \theta \end{bmatrix} \begin{bmatrix} r \\ s \end{bmatrix}$$

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Projections



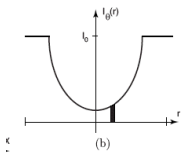
$$I_0(r) = I_0 \exp\left(-\int_{L,r,\theta} \mu(x,y) ds\right)$$

$$= I_0 \exp\left(-\int_{L,r,\theta} \mu(r \cos \theta - s \sin \theta, r \sin \theta + s \cos \theta) ds\right)$$

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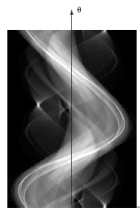
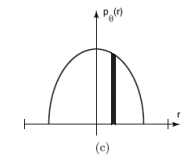
Projections



$$I_0(r) = I_0 \exp\left(-\int_{L,r,\theta} \mu(r \cos \theta - s \sin \theta, r \sin \theta + s \cos \theta) ds\right)$$

$$p_0(r) = -\ln \frac{I_0(r)}{I_0}$$

$$= \int_{L,r,\theta} \mu(r \cos \theta - s \sin \theta, r \sin \theta + s \cos \theta) ds$$

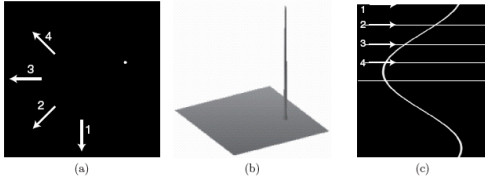


Sinogram

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Sinogram



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Systems 2002

Direct Inverse Approach

μ_1	μ_2
μ_3	μ_4

$$\begin{matrix} p_1 & p_1 = \mu_1 + \mu_2 \\ p_2 & p_2 = \mu_3 + \mu_4 \\ p_3 & p_3 = \mu_1 + \mu_3 \\ p_4 & p_4 = \mu_2 + \mu_4 \end{matrix} \quad \begin{bmatrix} p_1 \\ p_2 \\ p_3 \\ p_4 \end{bmatrix} = \begin{bmatrix} 1 & 1 & 0 & 0 \\ 0 & 0 & 1 & 1 \\ 1 & 0 & 1 & 0 \\ 0 & 1 & 0 & 1 \end{bmatrix} \begin{bmatrix} \mu_1 \\ \mu_2 \\ \mu_3 \\ \mu_4 \end{bmatrix}$$

4 equations, 4 unknowns.
Are these the correct equations to use?

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Direct Inverse Approach

μ_1	μ_2
μ_3	μ_4

$$\begin{matrix} p_1 & p_1 = \mu_1 + \mu_2 \\ p_2 & p_2 = \mu_3 + \mu_4 \\ p_3 & p_3 = \mu_1 + \mu_3 \\ p_4 & p_4 = \mu_2 + \mu_4 \\ p_5 & p_5 = \mu_1 + \mu_4 \end{matrix} \quad \begin{bmatrix} p_1 \\ p_2 \\ p_3 \\ p_4 \\ p_5 \end{bmatrix} = \begin{bmatrix} 1 & 1 & 0 & 0 \\ 0 & 0 & 1 & 1 \\ 1 & 0 & 1 & 0 \\ 0 & 1 & 0 & 1 \\ 1 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} \mu_1 \\ \mu_2 \\ \mu_3 \\ \mu_4 \end{bmatrix}$$

4 equations, 4 unknowns. These are linearly independent now.
In general for a $N \times N$ image, N^2 unknowns, N^2 equations.
This requires the inversion of a $N^2 \times N^2$ matrix
For a high-resolution 512×512 image, $N^2 = 262144$ equations.
Requires inversion of a 262144×262144 matrix!
Inversion process sensitive to measurement errors.

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**Iterative Inverse Approach
Algebraic Reconstruction Technique (ART)**

1	2	3	2.5	2.5	5
3	4	7	2.5	2.5	5
4	6	5	↓		
1	2	3	1.5	1.5	3
3	4	7	3.5	3.5	7
5	5		5	5	

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Backprojection

0	0	0	0
0	0	0	0
0	0	0	0

3 0 3 0 3

0	0	0
1	1	1
0	0	0

→

1	0	0
1	2	1
0	0	1

→

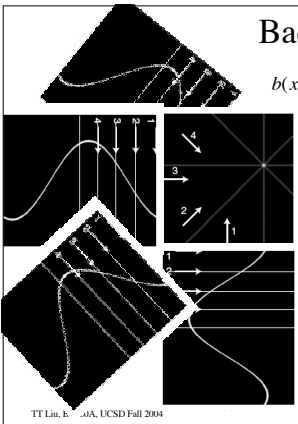
1	1	0
1	3	1
0	1	1

→

1	1	1
1	4	1
1	1	1

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Backprojection

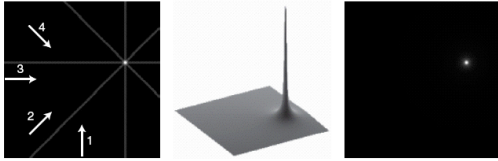


$$b(x,y) = B\{p(r,\theta)\}$$

$$= \int_0^\pi p(x \cos \theta + y \sin \theta, \theta) d\theta$$

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Backprojection

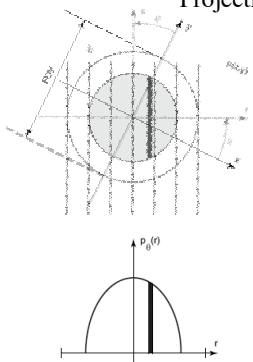


$$b(x, y) = B\{p(r, \theta)\} = \int_0^\pi p(x \cos \theta + y \sin \theta, \theta) d\theta$$

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Projection Theorem

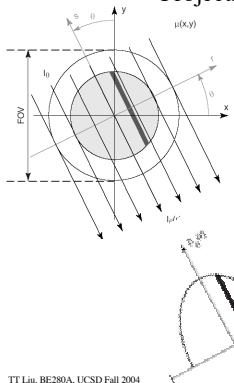


$$\begin{aligned} U(k_x, 0) &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \mu(x, y) e^{-j2\pi(k_x x + k_y y)} dx dy \\ &= \int_{-\infty}^{\infty} \left[\int_{-\infty}^{\infty} \mu(x, y) dy \right] e^{-j2\pi k_x x} dx \\ &= \int_{-\infty}^{\infty} p_0(x) e^{-j2\pi k_x x} dx \\ &= \int_{-\infty}^{\infty} p_0(r) e^{-j2\pi k r} dr \end{aligned}$$

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Projection Theorem



$$\begin{aligned} U(k_x, k_y) &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \mu(x, y) e^{-j2\pi(k_x x + k_y y)} dx dy \\ &= F_{2D}[\mu(x, y)] \end{aligned}$$

$$U(k_x, k_y) = P(k, \theta)$$

$$k_x = k \cos \theta$$

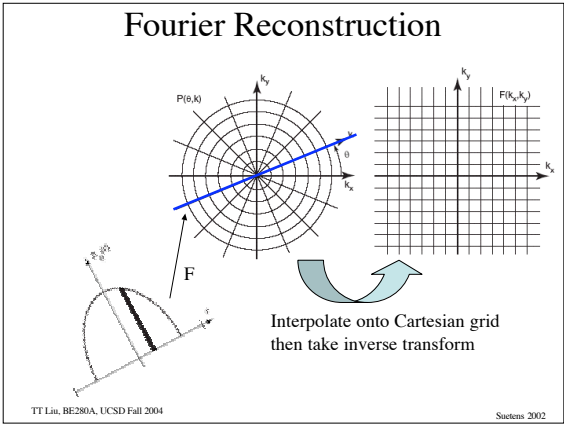
$$k_y = k \sin \theta$$

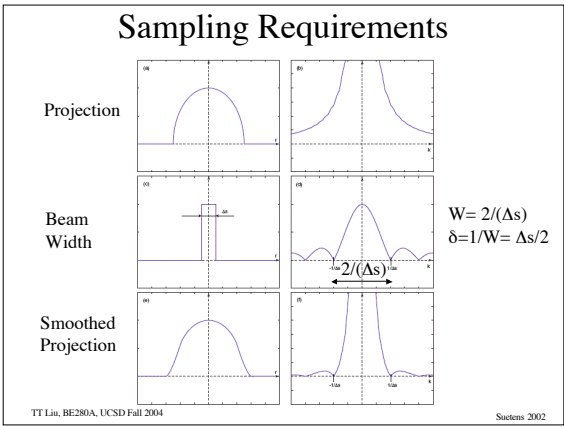
$$k = \sqrt{k_x^2 + k_y^2}$$

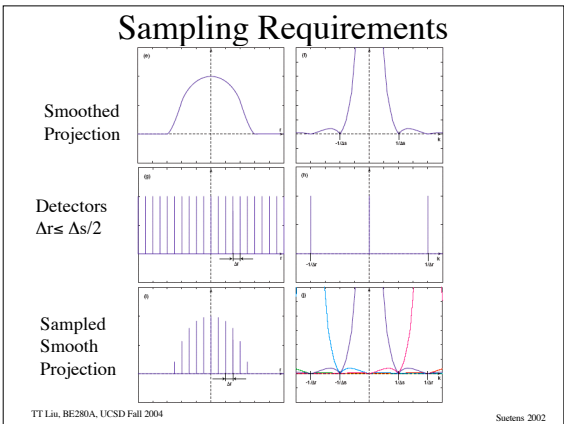
$$P(k, \theta) = \int_{-\infty}^{\infty} p_0(r) e^{-j2\pi k r} dr$$

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Sampling Requirements

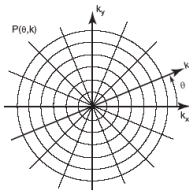
Size of detector $\Delta r = \delta = 1/W = \Delta s/2$
 Number of Detectors $N = \text{FOV} / \Delta r$ where $\Delta r \leq \Delta s/2$

Angular Sampling -- how many views?
 Want Circumference/(views in 360 degrees) = Δr
 $\pi \text{FOV} / (\text{views}) = \Delta r = \text{FOV} / N$
 Number of views in 360 degrees = πN

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Polar Version of Inverse FT



$$\begin{aligned} \mu(x, y) &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} U(k_x, k_y) e^{j2\pi(k_x x + k_y y)} dk_x dk_y \\ &= \int_0^{2\pi} \int_0^{\infty} U(k, \theta) e^{j2\pi(k \cos \theta x + k \sin \theta y)} k dk d\theta \\ &= \int_0^{\pi} \int_{-\infty}^{\infty} U(k, \theta) e^{j2\pi(xk \cos \theta + yk \sin \theta)} |k| dk d\theta \end{aligned}$$

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Filtered Backprojection

$$\begin{aligned} \mu(x, y) &= \int_0^{\pi} \int_{-\infty}^{\infty} U(k, \theta) e^{j2\pi(xk \cos \theta + yk \sin \theta)} |k| dk d\theta \\ &= \int_0^{\pi} \int_{-\infty}^{\infty} |k| U(k, \theta) e^{j2\pi k r} dk d\theta \\ &= \int_0^{\pi} u^*(r, \theta) d\theta \quad \leftarrow \text{Backproject a filtered projection} \end{aligned}$$

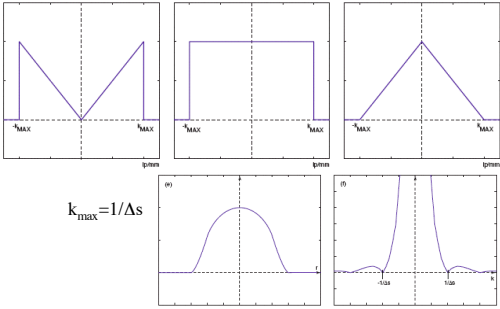
where $r = x \cos \theta + y \sin \theta$

$$\begin{aligned} u^*(r, \theta) &= \int_{-\infty}^{\infty} |k| U(k, \theta) e^{j2\pi k r} dk \\ &= u(r, \theta) * F^{-1}[|k|] \\ &= u(r, \theta) * q(r) \end{aligned}$$

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Ram-Lak Filter



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Additional Filtering

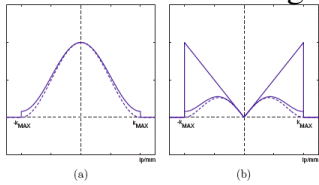


Figure 5.12: (a) Hamming window with $\alpha = 0.54$ and Hanning window (dashed) with $\alpha = 0.5$. (b) Ramp filter and its products with a Hamming window and a Hanning window (dashed).

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