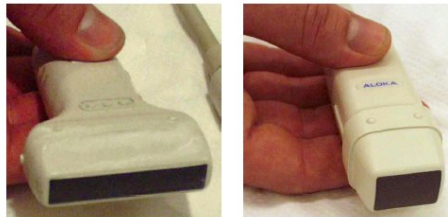


Bioengineering 280A
Principles of Biomedical Imaging

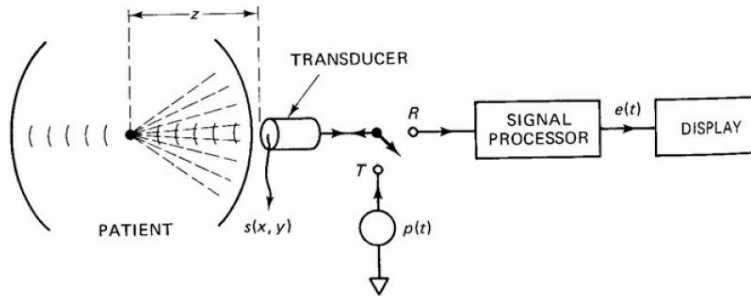
Fall Quarter 2006
Ultrasound Lecture 1

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Basic System

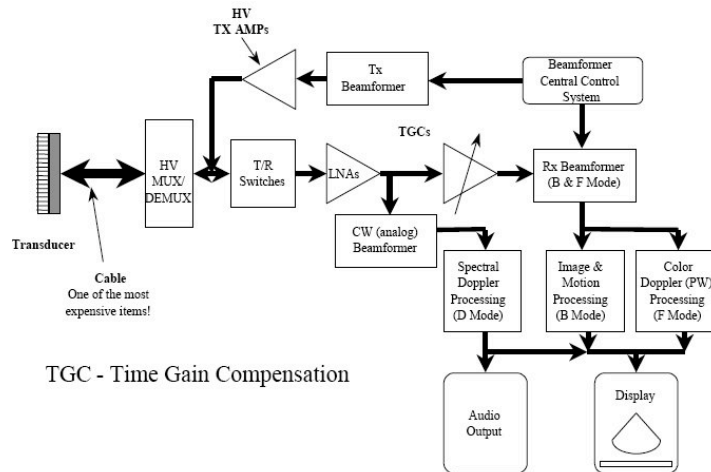


Echo occurs at $t=2z/c$ where c is approximately 1500 m/s or 1.5 mm/ μ s

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Macovski 1983

Basic System

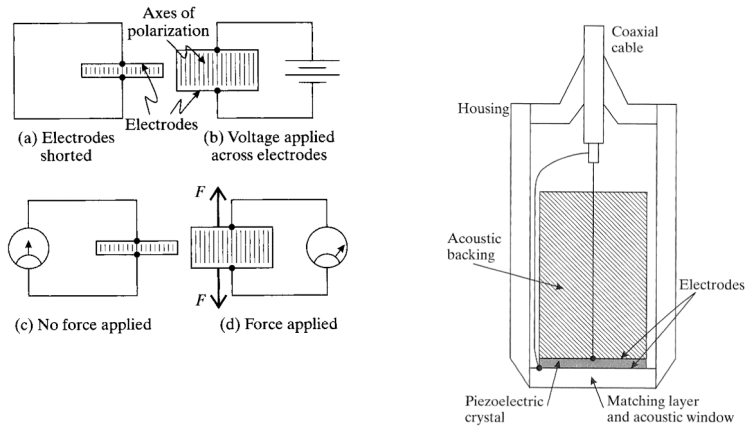


TGC - Time Gain Compensation

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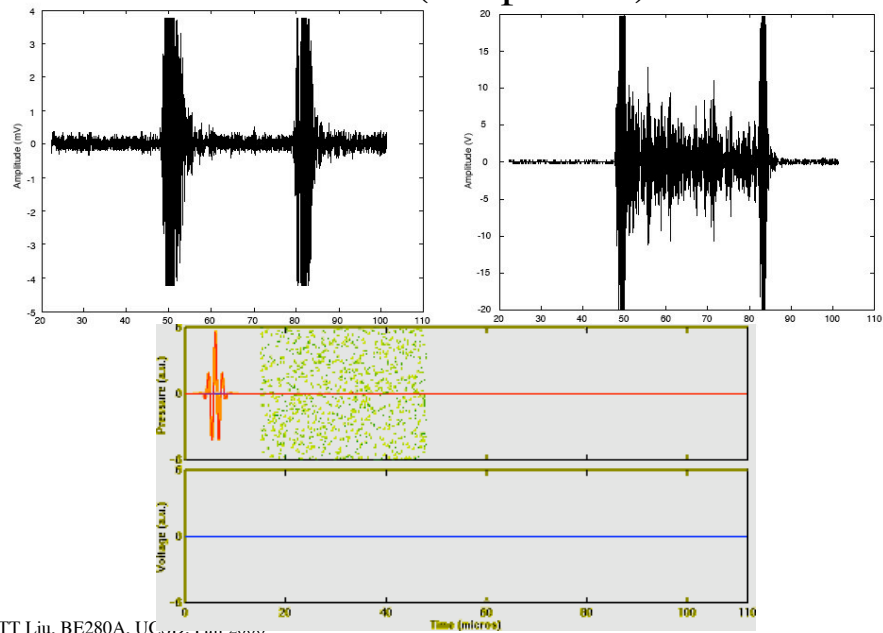
Transducer



Prince and Links 2006

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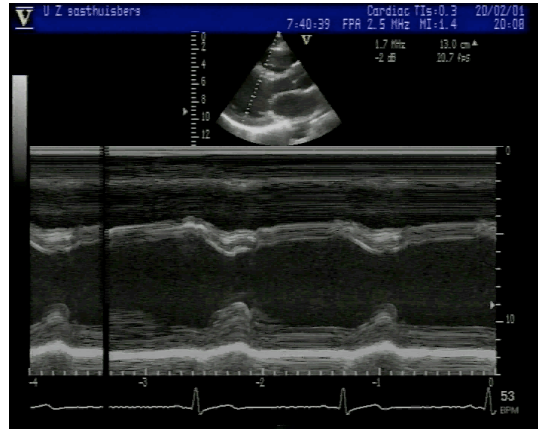
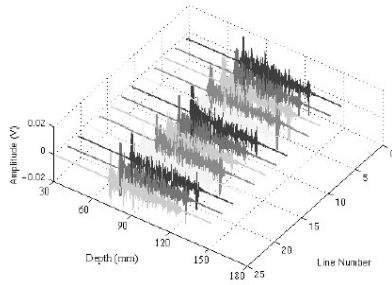
A-Mode (Amplitude)



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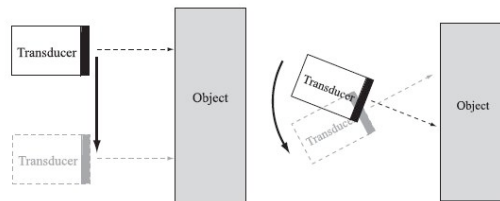
M-Mode (Motion)



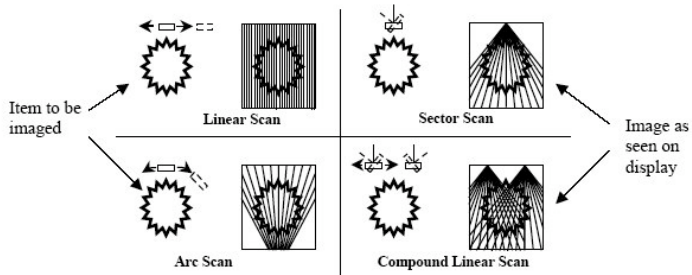
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B-Mode (Brightness)



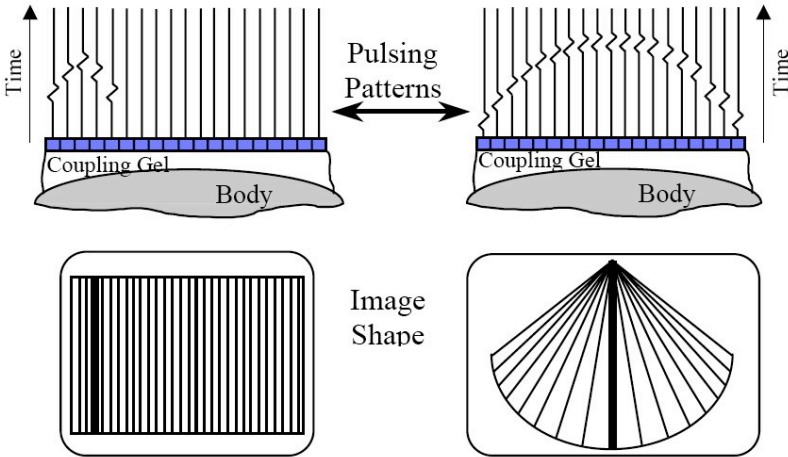
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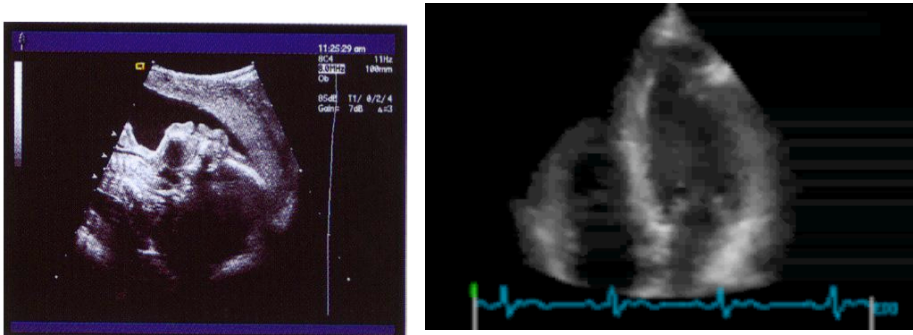
B-Mode (Brightness)



Brunner 2002

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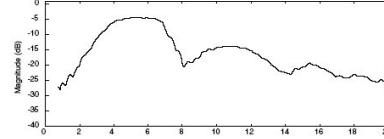
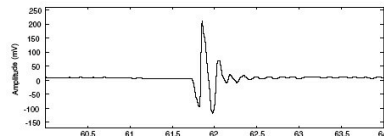
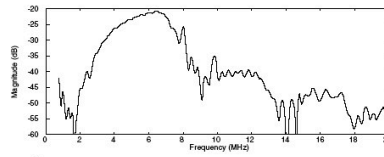
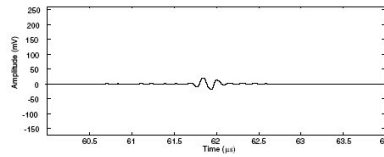
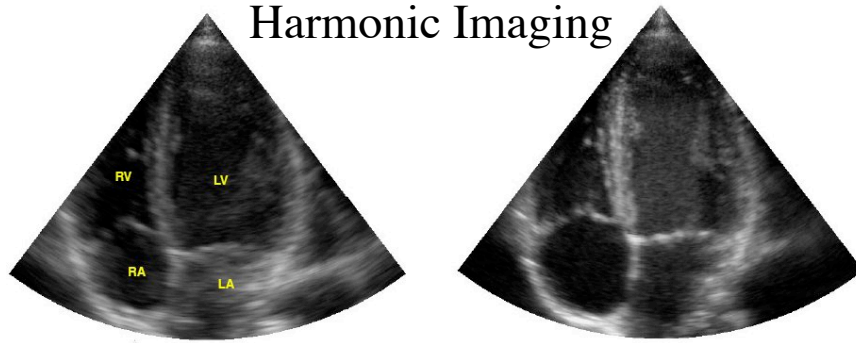
B-Mode



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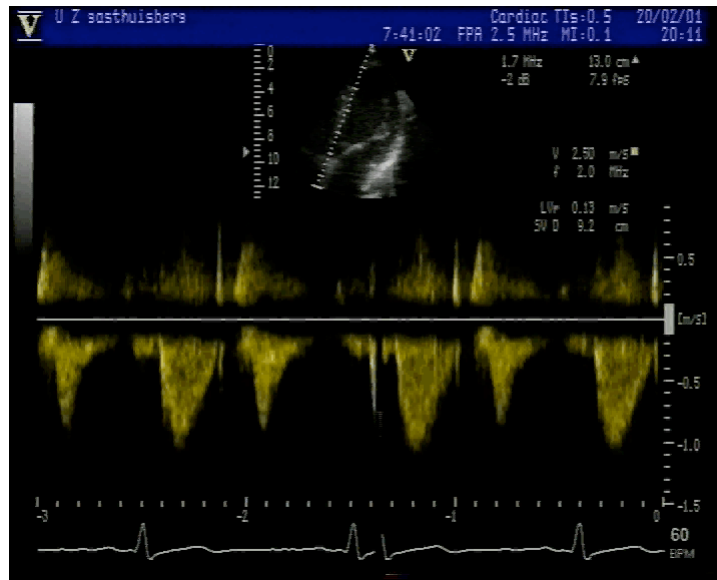
Harmonic Imaging



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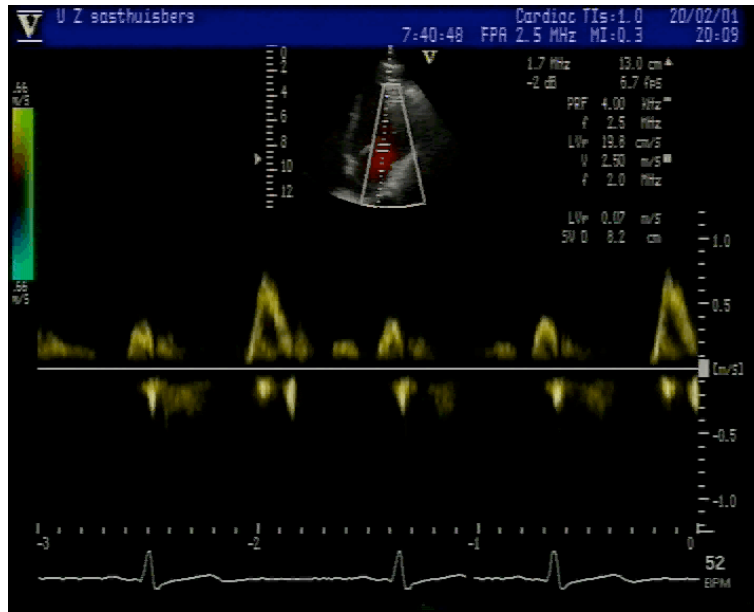
CW Doppler Imaging



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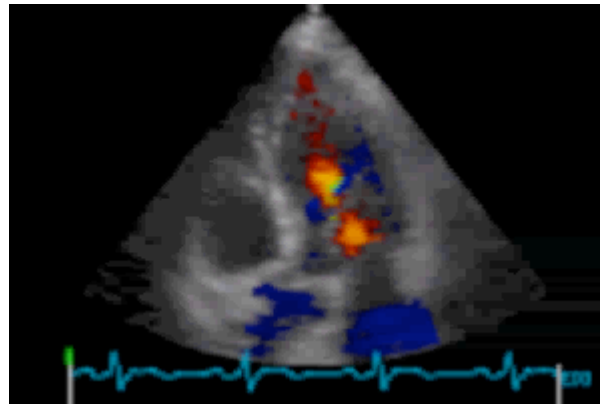
PW Doppler Imaging



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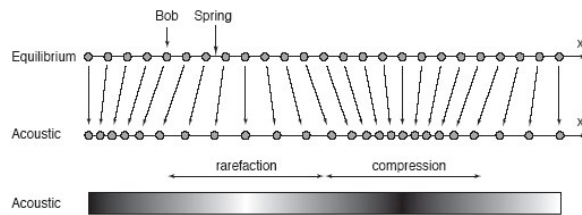
Color Doppler Imaging



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Acoustic Waves



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Speed of Sound

$$c = \sqrt{\frac{1}{\kappa\rho}} \quad [\text{m s}^{-1}]$$

κ = compressibility $[\text{m s}^2 \text{kg}^{-1}] = [1/\text{Pascal}]$

ρ = density $[\text{kg m}^{-3}]$

Material	Density	Speed m/s
Air	1.2	330
Water	1000	1480
Bone	1380-1810	4080
Fat	920	1450
Liver	1060	1570

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Impedance

$$\text{Impedance } Z = \frac{\text{Pressure}}{\text{Velocity}} = \frac{P}{v} = \rho c = \sqrt{\frac{\rho}{\kappa}}$$

density kg/m³
speed of sound

- Brain 1541 m/s
- Liver 1549
- Skull bone 4080 m/s
- Water 1480 m/s

Note: particle velocity and speed of sound are not the same!

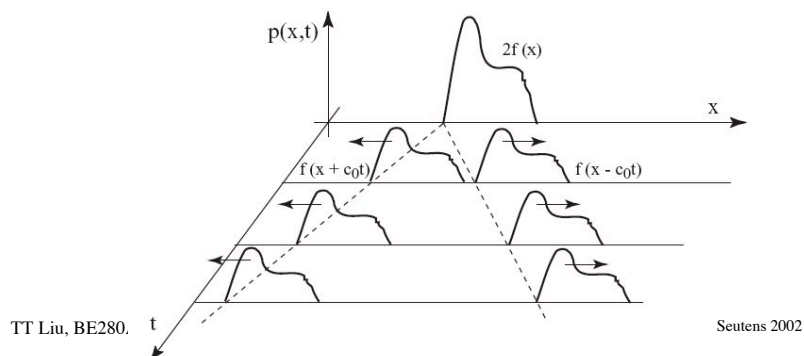
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Acoustic Wave Equation

$$\nabla^2 p = \left(\frac{\partial^2}{\partial x^2} + \frac{\partial^2}{\partial y^2} + \frac{\partial^2}{\partial z^2} \right) p = \frac{1}{c^2} \frac{\partial^2 p}{\partial t^2}$$

Solutions are of the form

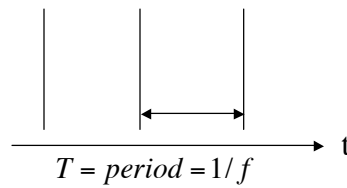
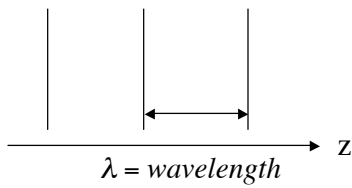
$$p(x,t) = A_1 f_1(x - ct) + A_2 f_2(x + ct)$$



Plane Waves

$$\begin{aligned}
 p(z,t) &= \cos(k(z-ct)) \\
 &= \cos\left(\frac{2\pi}{\lambda}(z-ct)\right) \\
 &= \cos\left(\frac{2\pi f}{c}(z-ct)\right) \\
 &= \cos(2\pi f(z/c-t))
 \end{aligned}$$

$$\begin{aligned}
 p(z,t) &= \exp(jk(z-ct)) \\
 k = \text{wavenumber} &= \frac{2\pi}{\lambda} = 2\pi k_z \\
 \lambda = \text{wavelength} &= \frac{c}{f} \\
 f = \text{frequency} & \text{ [cycles/sec]} \\
 T = \text{period} &= \frac{1}{f}
 \end{aligned}$$



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Spherical Waves

$$p(r,t) = \frac{1}{r} \phi(t-r/c) + \frac{1}{r} \phi(t+r/c)$$

Outward wave
Inward wave

Outward wave

$$p(r,t) = \frac{1}{r} \exp(j2\pi f(t-r/c))$$



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Acoustic Intensity

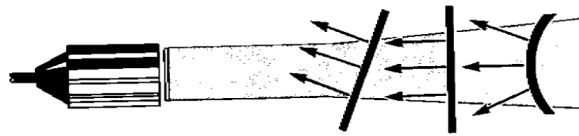
$$I = pv$$
$$= \frac{p^2}{Z}$$

Also called acoustic energy flux.
Analogous to electric power

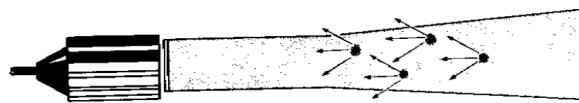
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Echos

SPECULAR ECHOES

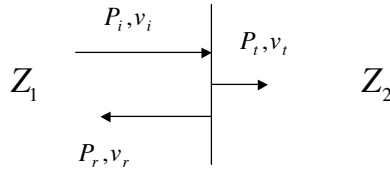


SCATTERED ECHOES



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Specular Reflection



Material	Reflectivity
Brain-skull	0.66
Fat-muscle	0.10
Muscle-blood	0.03
Soft-tissue-air	.9995

$$v_i - v_r = v_t \quad (\text{velocity boundary condition})$$

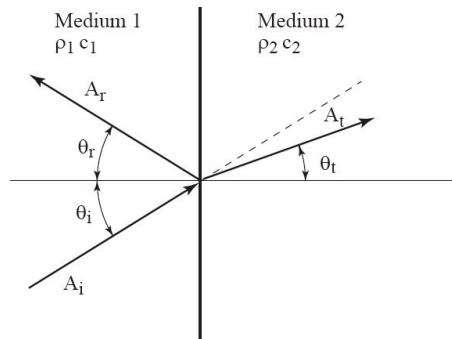
$$\frac{P_i}{Z_1} - \frac{P_r}{Z_1} = \frac{P_t}{Z_2}$$

$$P_i + P_r = P_t \quad (\text{pressure boundary condition})$$

$$R = \frac{P_r}{P_i} = \frac{Z_2 - Z_1}{Z_2 + Z_1} \approx \frac{\Delta Z}{Z_0}$$

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Reflection and Refraction



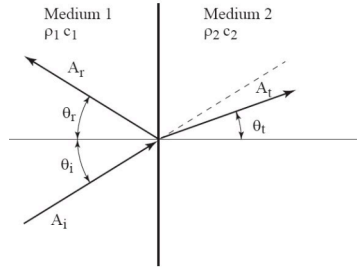
Snell's Law

$$\frac{\sin \theta_i}{c_1} = \frac{\sin \theta_r}{c_1} = \frac{\sin \theta_t}{c_2}$$

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Reflection and Refraction



$$v_i \cos \theta_i = v_r \cos \theta_r + v_t \cos \theta_t$$

$$\frac{p_i}{Z_1} \cos \theta_i = \frac{p_r}{Z_1} \cos \theta_r + \frac{p_t}{Z_2} \cos \theta_t$$

$$p_i + p_r = p_t$$

Pressure Reflectivity

$$R = \frac{p_r}{p_i} = \frac{Z_2 \cos \theta_i - Z_1 \cos \theta_t}{Z_2 \cos \theta_i + Z_1 \cos \theta_t}$$

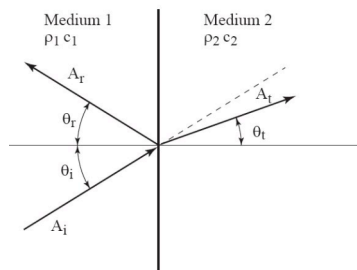
Pressure Transmittivity

$$T = \frac{p_t}{p_i} = \frac{2Z_2 \cos \theta_i}{Z_2 \cos \theta_i + Z_1 \cos \theta_t}$$

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Reflection and Refraction



Intensity Reflectivity

$$R_I = \frac{I_r}{I_i} = \frac{p_r^2}{p_i^2} = \left(\frac{Z_2 \cos \theta_i - Z_1 \cos \theta_t}{Z_2 \cos \theta_i + Z_1 \cos \theta_t} \right)^2$$

Intensity Transmittivity

$$T_I = \frac{I_t}{I_i} = \frac{p_t^2 Z_1}{p_i^2 Z_2} = \frac{4Z_1 Z_2 \cos^2 \theta_i}{(Z_2 \cos \theta_i + Z_1 \cos \theta_t)^2}$$

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Example

Example : Fat/liver interface at normal incidence

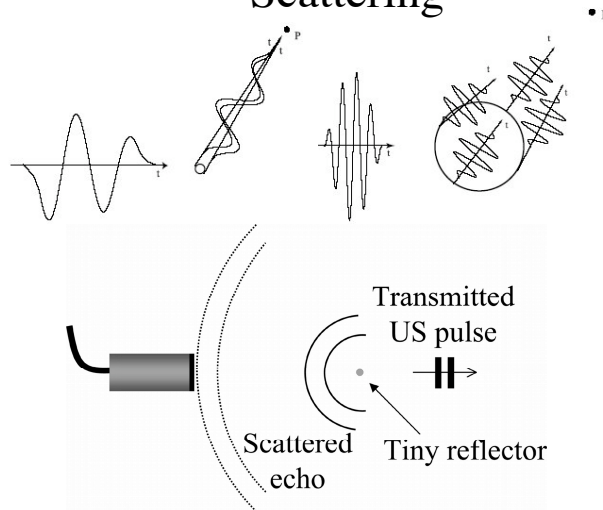
$$Z_{fat} = 1.35 \times 10^{-6} \text{ kg m}^{-2} \text{ s}^{-1}$$

$$Z_{liver} = 1.66 \times 10^{-6} \text{ kg m}^{-2} \text{ s}^{-1}$$

$$R_I = \left(\frac{Z_{liver} - Z_{fat}}{Z_{liver} + Z_{fat}} \right)^2 = 0.103$$

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Scattering



Point scatterers retransmit the incident wave equally in all direction (e.g. isotropic scattering).

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Attenuation

Loss of acoustic energy during propagation.

Conversion of acoustic energy into heat.

$$\begin{aligned} p(z,t) &= A_z f(t - c/z) \\ &= A_0 \exp(-\mu_a z) f(t - c/z) \end{aligned}$$

Amplitude attenuation factor

$$\mu_a = -\frac{1}{z} \ln \frac{A_z}{A_0} \quad : \text{ units = nepers/cm}$$

$$\alpha = -20 \frac{1}{z} \log_{10} \frac{A_z}{A_0} = 20 \mu_a \log_{10}(e) \approx 8.7 \mu_a \quad : \text{ dB/cm}$$

↑
Attenuation coefficient

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Attenuation

$$\alpha(f) = \alpha_0 f^n$$

For frequencies used in medical ultrasound, $n \approx 1$.

$$\alpha(f) \approx \alpha_0 f$$

Material	α_0 [dB/cm/MHz]
fat	0.63
liver	0.94
Cardiac muscle	1.8
bone	20.0

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Example

Example : Fat at 5 MHz

$$\begin{aligned} \text{Attenuation coefficient} &= 5\text{MHz} \times 0.63 \text{ dB/cm/MHz} \\ &= 3.15\text{dB/cm} \end{aligned}$$

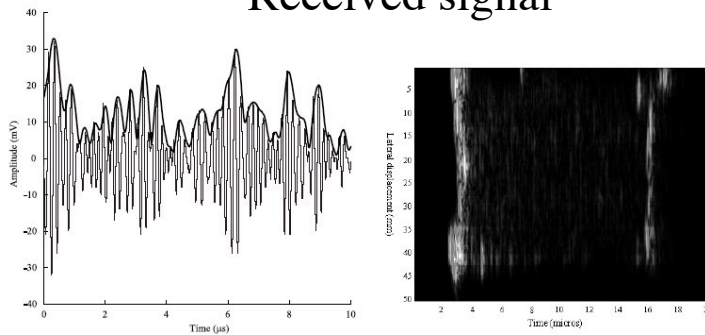
After 4 cm, attenuation = $4 * 3.15 = 12.6 \text{ dB}$

Relative amplitude is $10^{(-12.6/20)} = 0.2344$

$$\text{Recall dB} \equiv 20\log_{10}(A_z / A_0)$$

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Received signal

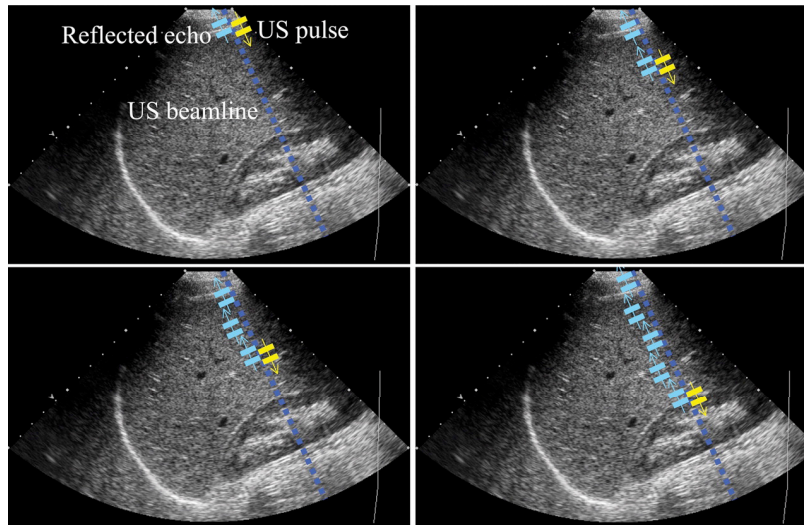


$$e(t) = K \int \int \int \frac{e^{-2\alpha z}}{z} R(x, y, z) s(x, y) p(t - 2z/c) dx dy dz$$

↑ Attenuation
 ↑ Reflection/Scattering
 ↑ Beam width
 ↑ Pulse

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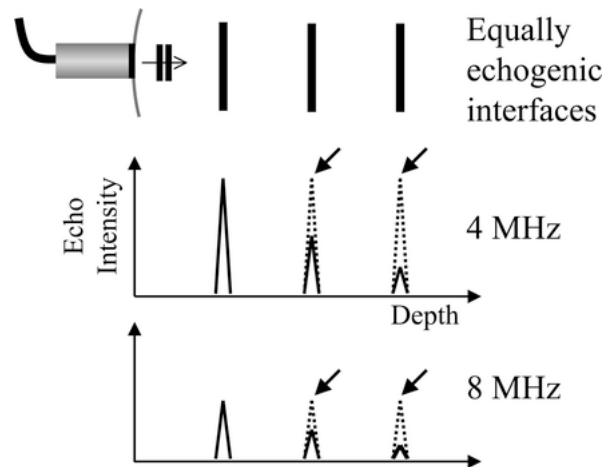
Received signal



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<http://radiographics.rsna.org/content/vol23/issue4/images/large/g03jl25c1x.jpeg>

Attenuation Correction



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Attenuation Correction and Signal Equation

$$e(t) = K \int \int \int \frac{e^{-2\alpha z}}{z} R(x, y, z) s(x, y) p(t - 2z/c) dx dy dz$$

$$\approx K \frac{e^{-\alpha ct}}{ct/2} \int \int \int R(x, y, z) s(x, y) p(t - 2z/c) dx dy dz$$

$$e_c(t) = cte^{\alpha ct} e(t)$$

$$\approx K \int \int \int R(x, y, z) s(x, y) p(t - 2z/c) dx dy dz$$

$$= \frac{c}{2} \int \int \int R(x, y, c\tau/2) s(x, y) p(t - \tau) dx dy d\tau$$

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Impulse Response

Transducer centered at 0,0 (defines image at 0,0)

$$e_c(t) = K \int \int \int R(x, y, z) s(x, y) p(t - 2z/c) dx dy dz$$

$$= K \int \int \int \delta(x, y, z - z_0) s(x, y) p(t - 2z/c) dx dy dz$$

$$= Ks(0,0) p(t - 2z_0/c)$$

Transducer centered at x_0, y_0 (defines image at these coordinates)

$$e_c(t) = K \int \int \int R(x, y, z) s(x - x_0, y - y_0) p(t - 2z/c) dx dy dz$$

$$= K \int \int \int \delta(x, y, z - z_0) s(x - x_0, y - y_0) p(t - 2z/c) dx dy dz$$

$$= Ks(-x_0, -y_0) p(t - 2z_0/c)$$

Lateral Response is therefore $s(-x, -y)$

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Impulse Response

Depth response

$$\begin{aligned} p(t - 2z_0/c) &= p(2z/c - 2z_0/c) \\ &= p\left(\frac{2(z - z_0)}{c}\right) \end{aligned}$$

Therefore impulse response is simply

$p(t)$ in the time domain or

$p(2z/c)$ in the spatial domain

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Signal Equation

In general, we can write

$$\begin{aligned} e_c(t, x_0, y_0) &= K \int \int \int R(x, y, z) s(x - x_0, y - y_0) p(t - 2z/c) dx dy dz \\ &= K \frac{c}{2} [R(x, y, ct/2) *** s(-x, -y) p(t)] \Big|_{x=x_0, y=y_0} \end{aligned}$$

$$\begin{aligned} e_c(z', x_0, y_0) &= K \int \int \int R(x, y, z) s(x - x_0, y - y_0) p(2(z' - z)/c) dx dy dz \\ &= [R(x, y, z') *** s(-x, -y) p(2z'/c)] \Big|_{x=x_0, y=y_0} \end{aligned}$$

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Depth Resolution

$p(t) = p(2z/c)$ determines the depth resolution

Pulses are of the form $a(t) \cos(2\pi f_0 t + \theta)$ where $a(t)$ is the envelope function and f_0 is the resonant frequency of the transducer.

The duration of T of $a(t)$ is typically chosen to be about 2 or 3 periods (e.g. $T = 3/f_0$). If the duration is too short, the bandwidth of the pulse will be very large and much of its power will be attenuated.

The depth resolution is approximately $\Delta z = cT/2 \approx 1.5c / f_0 = 1.5\lambda$.

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Depth Resolution

The depth resolution is approximately $\Delta z = cT/2 \approx 1.5c / f_0 = 1.5\lambda$.

Example :

For $f_0 = 5$ MHz, $\Delta z = (1.5)(1500 \text{ m/s}) / (5 \times 10^6 \text{ Hz}) = 0.45 \text{ mm}$

Trade - off

Higher $f_0 \Rightarrow$ Smaller $\Delta z \Rightarrow$ but more attenuation

Example : Assume 1dB/cm/MHz

For 10 cm depth, 20 cm roundtrip path length.

At 1 MHz 20 dB of attenuation \Rightarrow Attenuation = 0.1

At 10 MHz 200 dB of attenuation \Rightarrow Attenuation = 1×10^{-10}

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