

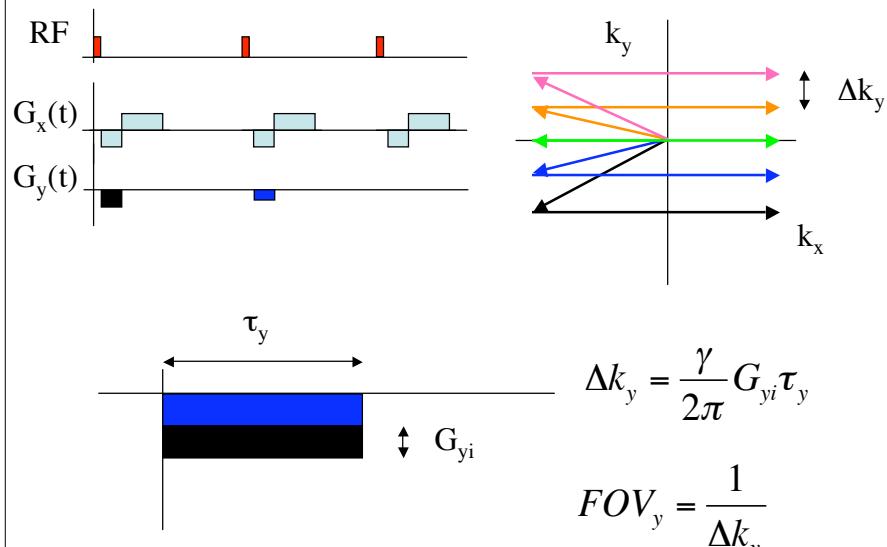
Bioengineering 280A

Principles of Biomedical Imaging

Fall Quarter 2006
MRI Lecture 3a

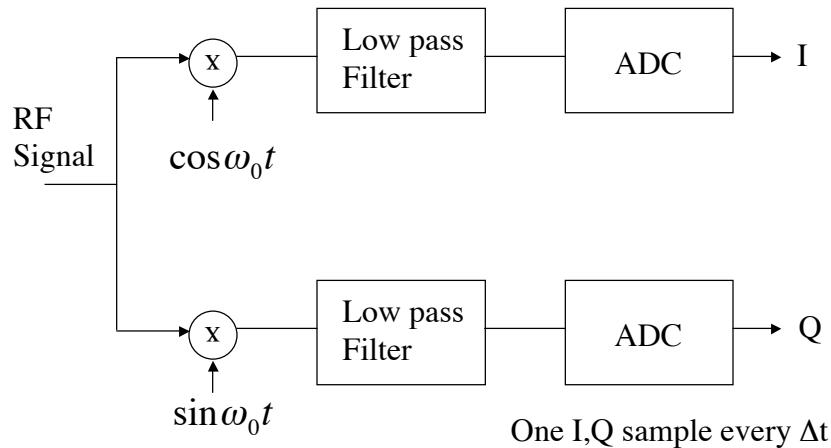
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Sampling in k_y



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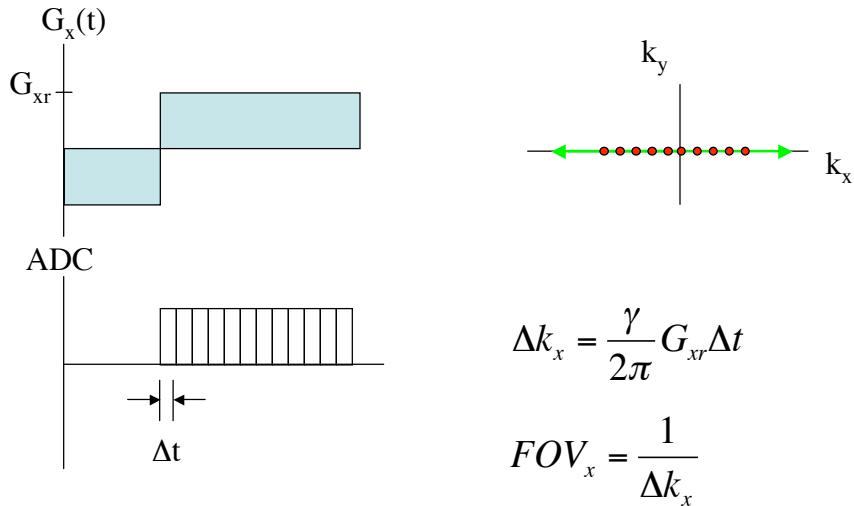
Sampling in k_x



Note: In practice, there are number of ways of
implementing this processing.

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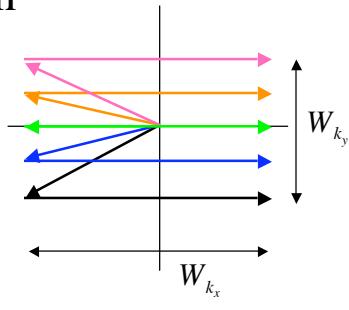
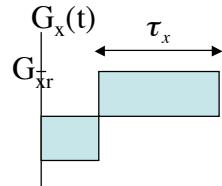
Sampling in k_x



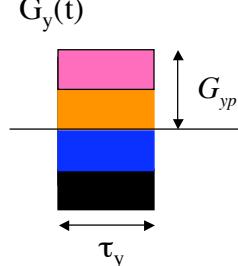
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Resolution

$$\delta_x = \frac{1}{W_{k_x}} = \frac{1}{2k_{x,\max}} = \frac{1}{\frac{\gamma}{2\pi} G_{xr} \tau_x}$$



$$\delta_y = \frac{1}{W_{k_y}} = \frac{1}{2k_{y,\max}} = \frac{1}{\frac{\gamma}{2\pi} 2G_{yp} \tau_y}$$



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Example

Goal :

$$FOV_x = FOV_y = 25.6 \text{ cm}$$

$$\delta_x = \delta_y = 0.1 \text{ cm}$$

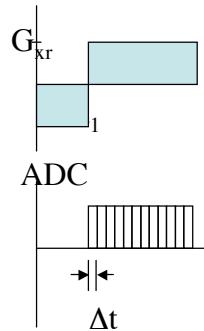
Readout Gradient :

$$FOV_x = \frac{1}{\frac{\gamma}{2\pi} G_{xr} \Delta t}$$

Pick $\Delta t = 32 \mu\text{sec}$

$$\begin{aligned} G_{xr} &= \frac{1}{FOV_x \frac{\gamma}{2\pi} \Delta t} = \frac{1}{(25.6\text{cm})(42.57 \times 10^6 T^{-1}s^{-1})(32 \times 10^{-6}\text{s})} \\ &= 2.8675 \times 10^{-5} \text{T/cm} \\ &= .28675 \text{ G/cm} \end{aligned}$$

$$1 \text{ Gauss} = 1 \times 10^{-4} \text{ Tesla}$$



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Example

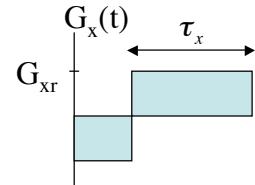
Readout Gradient :

$$\delta_x = \frac{1}{\frac{\gamma}{2\pi} G_{xr} \tau_x}$$

$$\begin{aligned}\tau_x &= \frac{1}{\delta_x \frac{\gamma}{2\pi} G_{xr}} = \frac{1}{(0.1cm)(4257 G^{-1}s^{-1})(0.28675 G/cm)} \\ &= 8.192 \text{ ms} \\ &= N_{\text{read}} \Delta t\end{aligned}$$

where

$$N_{\text{read}} = \frac{FOV_x}{\delta_x} = 256$$



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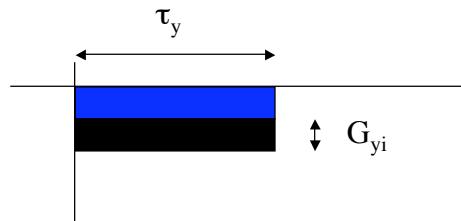
Example

Phase - Encode Gradient :

$$FOV_y = \frac{1}{\frac{\gamma}{2\pi} G_{yi} \tau_y}$$

Pick $\tau_y = 4.096 \text{ msec}$

$$\begin{aligned}G_{yi} &= \frac{1}{FOV_y \frac{\gamma}{2\pi} \tau_y} = \frac{1}{(25.6cm)(42.57 \times 10^6 T^{-1}s^{-1})(4.096 \times 10^{-3}s)} \\ &= 2.2402 \times 10^{-7} \text{ T/cm} \\ &= .00224 \text{ G/cm}\end{aligned}$$



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Example

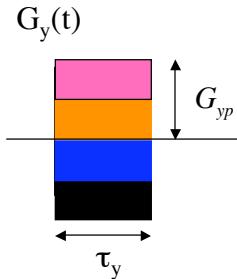
Phase - Encode Gradient :

$$\delta_y = \frac{1}{\frac{\gamma}{2\pi} 2G_{yp}\tau_y}$$

$$G_{yp} = \frac{1}{\delta_y 2 \frac{\gamma}{2\pi} \tau_y} = \frac{1}{(0.1cm)(4257 G^{-1}s^{-1})(4.096 \times 10^{-3} s)} \\ = 0.2868 \text{ G/cm} \\ = \frac{N_p}{2} G_{yi}$$

where

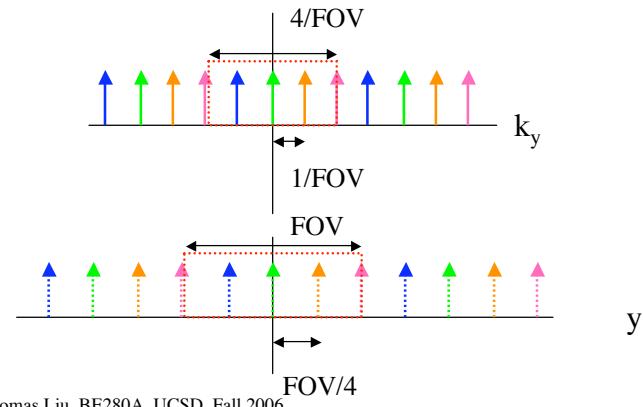
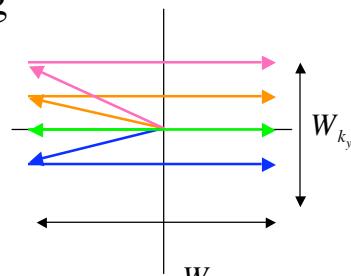
$$N_p = \frac{FOV_y}{\delta_y} = 256$$



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Sampling

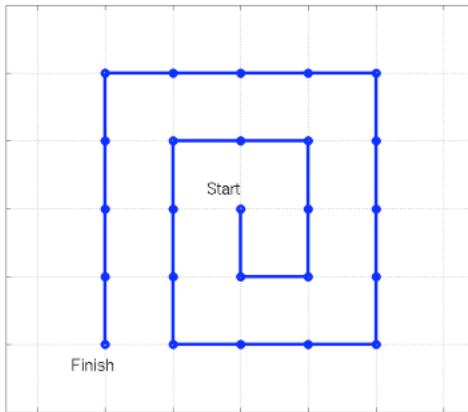
In practice, an even number (typically power of 2) sample is usually taken in each direction to take advantage of the Fast Fourier Transform (FFT) for reconstruction.



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Example

Consider the k-space trajectory shown below. ADC samples are acquired at the points shown with $\Delta t = 10 \mu\text{sec}$. The desired FOV (both x and y) is 10 cm and the desired resolution (both x and y) is 2.5 cm. Draw the gradient waveforms required to achieve the k-space trajectory. Label the waveform with the gradient amplitudes required to achieve the desired FOV and resolution. Also, make sure to label the time axis correctly.



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SCAN TIMING # of Echoes <input type="radio"/> 1 <input type="radio"/> 2 <input type="radio"/> 4 TE Min <input type="text" value="Full"/> <input type="button" value="▼"/> TE2 <input type="text"/> <input type="button" value="▼"/> TR <input type="text" value="750"/> <input type="button" value="▼"/> Inv. Time <input type="text"/> <input type="button" value="▼"/> TI2 <input type="text"/> <input type="button" value="▼"/> Flip Angle <input type="text"/> <input type="button" value="▼"/> Echo Train Length <input type="text"/> <input type="button" value="▼"/> Bandwidth <input type="text" value="25"/> <input type="button" value="▼"/> Bandwidth2 <input type="text"/> <input type="button" value="▼"/>	ACQUISITION TIMING Freq <input type="text" value="352"/> <input type="button" value="▼"/> Freq DIR <input type="radio"/> A/P <input type="radio"/> P/A Phase <input type="text" value="192"/> <input type="button" value="▼"/> Center Freq <input type="radio"/> Auto <input type="radio"/> Water NEX <input type="text" value="2.0"/> <input type="button" value="▼"/> Flow Comp <input type="radio"/> Off <input type="radio"/> On Phase FOV <input type="text" value="0.75"/> <input type="button" value="▼"/> <input type="checkbox"/> Autoshim <input type="checkbox"/> Phase Correct <input type="checkbox"/> Contrast Arterial <input type="text"/> # of Acqs Before <input type="text"/> <input type="button" value="▼"/> Agent <input type="text"/>
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SCANNING RANGE FOV <input type="text" value="22"/> <input type="button" value="▼"/> Slice Thickness <input type="text" value="5.0"/> <input type="button" value="▼"/> Spacing <input type="text" value="2.0"/> <input type="button" value="▼"/>	Start <input type="text"/> S/I <input type="button" value="▼"/> L/R Center <input type="text"/> <input type="button" value="▼"/> P/A Center <input type="text"/> <input type="button" value="▼"/> End <input type="text"/> <input type="button" value="▼"/> <input type="text"/> <input type="button" value="▼"/> <input type="text"/> <input type="button" value="▼"/> # Slices <input type="text"/> <input type="button" value="▼"/> Table Delta <input type="text"/> <input type="button" value="▼"/> Actual End <input type="text"/>
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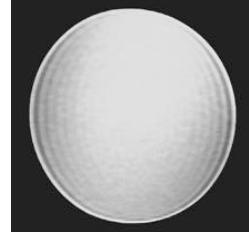
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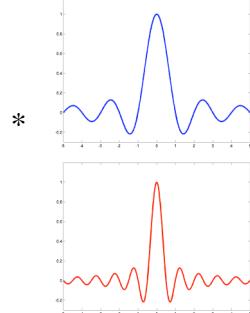
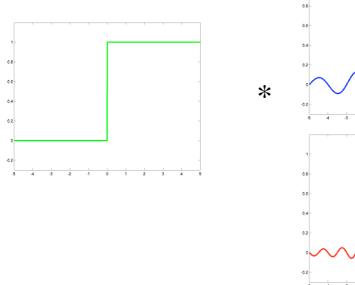
Gibbs Artifact



256x256 image

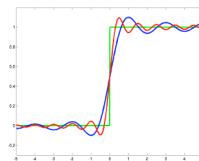


256x128 image



*

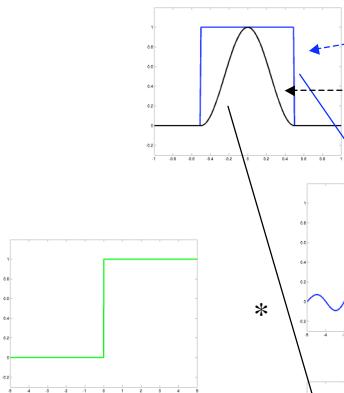
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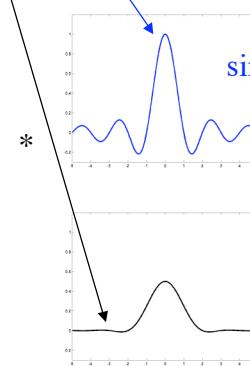
Images from <http://www.mritutor.org/mritutor/gibbs.htm>

Apodization



Hanning Window

$$h(k_x) = 1/2(1 + \cos(2\pi k_x))$$

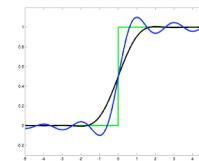


sinc(x)

*

$$0.5\text{sinc}(x) + 0.25\text{sinc}(x-1) \\ + 0.25\text{sinc}(x+1)$$

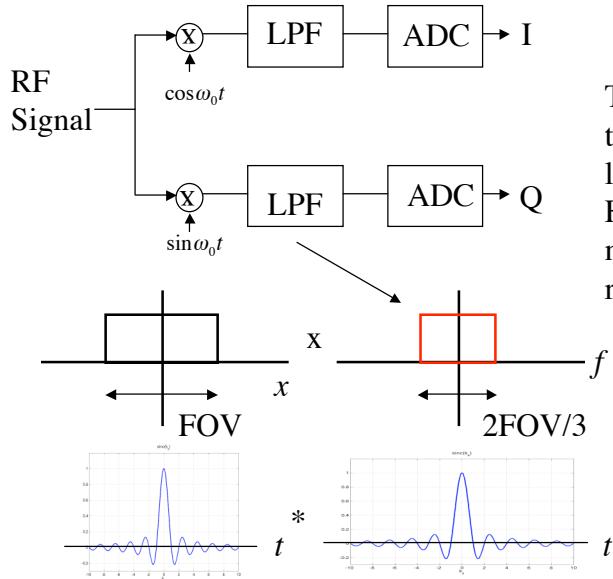
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Images from <http://www.mritutor.org/mritutor/gibbs.htm>

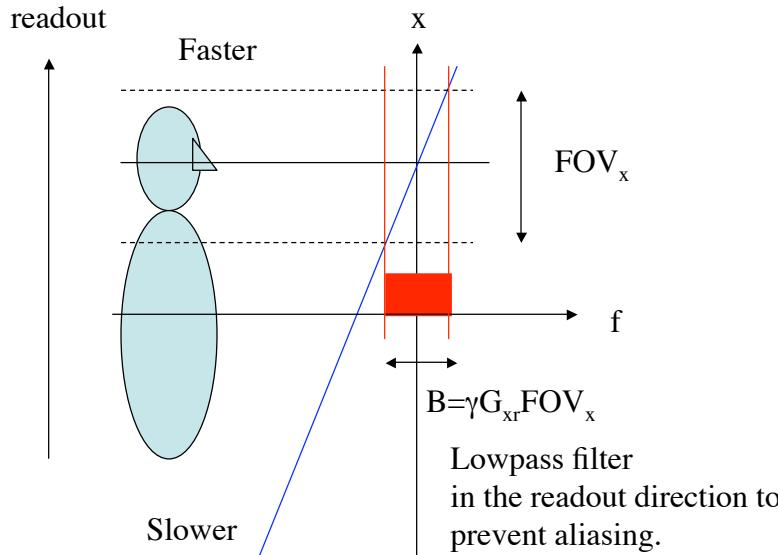
Aliasing and Bandwidth



Temporal filtering in the readout direction limits the readout FOV. So there should never be aliasing in the readout direction.

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Aliasing and Bandwidth



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Figure 7-31 Default Axial Directions

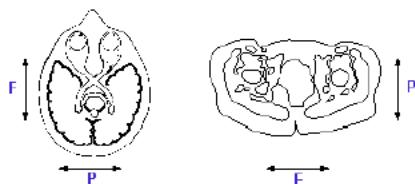
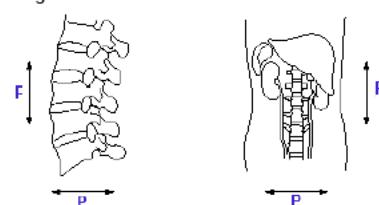


Figure 7-32 Default Sagittal and Coronal Directions



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