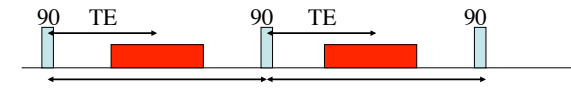


Bioengineering 280A
Principles of Biomedical Imaging

Fall Quarter 2015
MRI Lecture 5

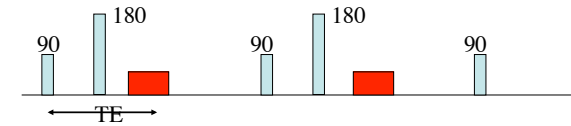
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Saturation Recovery Sequence



Gradient Echo

$$I(x, y) = \rho(x, y) \left[1 - e^{-TR/T_1(x, y)} \right] e^{-TE/T_2^*(x, y)}$$



Spin Echo

$$I(x, y) = \rho(x, y) \left[1 - e^{-TR/T_1(x, y)} \right] e^{-TE/T_2(x, y)}$$

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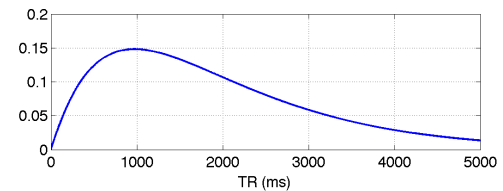
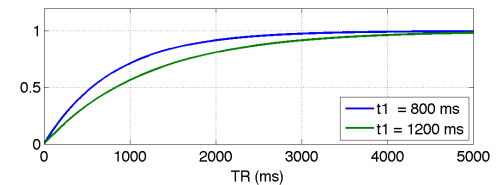
T1-Weighted Scans

Make TE very short compared to either T_2 or T_2^* . The resultant image has both proton and T_1 weighting.

$$I(x, y) \approx \rho(x, y) \left[1 - e^{-TR/T_1(x, y)} \right]$$

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T1-Weighted Scans



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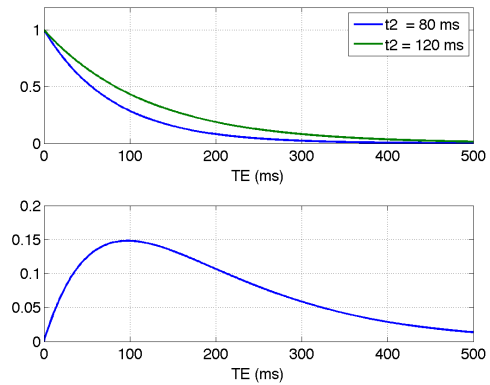
T2-Weighted Scans

Make TR very long compared to T_1 and use a spin-echo pulse sequence. The resultant image has both proton and T_2 weighting.

$$I(x, y) \approx \rho(x, y)e^{-TE/T_2}$$

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T2-Weighted Scans



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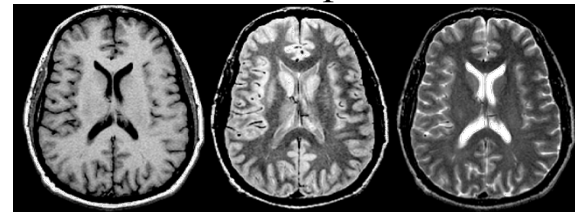
Proton Density Weighted Scans

Make TR very long compared to T_1 and use a very short TE. The resultant image is proton density weighted.

$$I(x, y) \approx \rho(x, y)$$

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Example



T₁-weighted

Density-weighted

T₂-weighted

Tissue	Proton Density	T1 (ms)	T2 (ms)
Csf	1.0	4000	2000
Gray	0.85	1350	110
White	0.7	850	80

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(a) Four images, all obtained with a common TR=5 seconds and TE=90, 50, 20, 15 ms (shown in reading order).

(b) Six images obtained with a common TE=15 ms and TR=500, 1000, 2000, 3000, 4000, 5000 ms (shown in reading order).

Figure 8: Phantom data which illustrates signal intensity and contrast for bottles filled with jello of varying consistency. Where is T_1 long/short? How long, how short? The same for T_2 ? Which bottles might be pure water? Which jello is most firm? What pictures are the most T_1 -, T_2 - and PD-weighted? Hanson 2009

1 2
3 4

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a) Which has the longest T_1 ?
 b) Which has the shortest T_1 ?
 c) Which has the longest T_2 ?
 d) Which has the shortest T_2 ?
 e) Which might be pure water?
 f) Which has the most firm jello?

(a) Four images, all obtained with a common TR=5 seconds and TE=90, 50, 20, 15 ms (shown in reading order).

(b) Six images obtained with a common TE=15 ms and TR=500, 1000, 2000, 3000, 4000, 5000 ms (shown in reading order).

Figure 8: Phantom data which illustrates signal intensity and contrast for bottles filled with jello of varying consistency. Where is T_1 long/short? How long, how short? The same for T_2 ? Which bottles might be pure water? Which jello is most firm? What pictures are the most T_1 -, T_2 - and PD-weighted? Hanson 2009

1 2
3 4
5 6 7
8 9 10

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a) Which is the most T_1 weighted?
 b) Which is the most T_2 weighted?
 c) Which is the most PD weighted?

FLASH sequence

Gradient Echo

$$I(x, y) = \rho(x, y) \frac{[1 - e^{-TR/T_1(x,y)}] \sin \theta}{[1 - e^{-TR/T_1(x,y)} \cos \theta]} \exp(-TE/T_2^*)$$

Signal intensity is maximized at the Ernst Angle

$$\theta_E = \cos^{-1}(\exp(-TR/T_1))$$

FLASH equation assumes no coherence from shot to shot. In practice this is achieved with RF spoiling.

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FLASH sequence

Flash signal intensity; $T_1 = 1000$ ms

Signal Intensity

Flip Angle

— TR = 30 ms
 — TR = 100 ms
 — TR = 500 ms

$$\theta_E = \cos^{-1}(\exp(-TR/T_1))$$

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Inversion Recovery

$$I(x, y) = \rho(x, y) \left[1 - 2e^{-TI/T_1(x, y)} + e^{-TR/T_1(x, y)} \right] e^{-TE/T_2(x, y)}$$

Intensity is zero when inversion time is

$$TI = -T_1 \ln \left[\frac{1 + \exp(-TR/T_1)}{2} \right]$$

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Inversion Recovery

Biglands *et al. Journal of Cardiovascular Magnetic Resonance*
2012 14:66 doi:10.1186/1532-429X-14-66

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Inversion Recovery

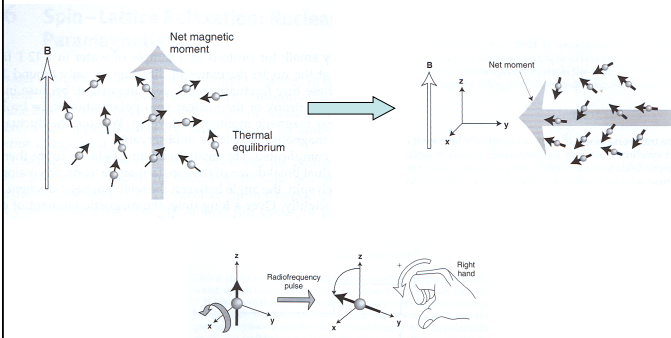
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Simplified Drawing of Basic Instrumentation.
Body lies on table encompassed by
coils for static field B_0 ,
gradient fields (two of three shown),
and radiofrequency field B_1 .

Image, caption: copyright Nishimura, Fig. 3.15

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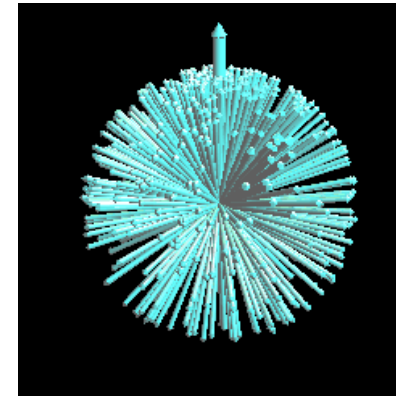
RF Excitation



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From Levitt, Spin Dynamics, 2001

RF Excitation



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<http://www.drcmr.dk/main/content/view/213/74/>

RF Excitation

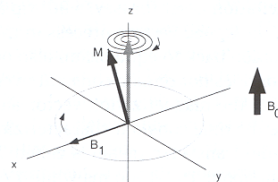


Image & caption: Nishimura, Fig. 3.2

At equilibrium, net magnetization is parallel to the main magnetic field. How do we tip the magnetization away from equilibrium?

B_1 radiofrequency field tuned to Larmor frequency and applied in transverse (xy) plane induces nutation (at Larmor frequency) of magnetization vector as it tips away from the z -axis.
- lab frame of reference

<http://www.eecs.umich.edu/~7Edno/BMES16/>

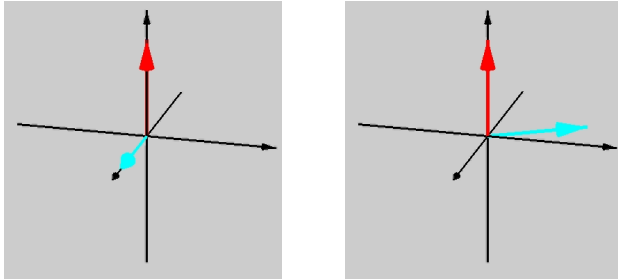
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<https://www.youtube.com/watch?v=kODOL-QBzSM>

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RF Excitation



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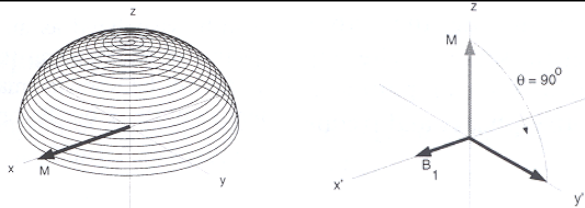
<http://www.eecs.umich.edu/%7EdnohBME516/>

Rotating Frame of Reference

Reference everything to the magnetic field at isocenter.

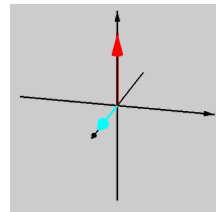


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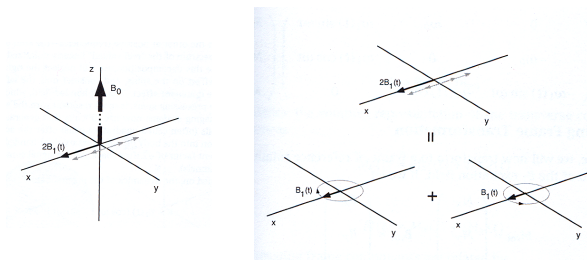
a) Laboratory frame behavior of \mathbf{M}
Images & caption: Nishimura, Fig. 3.3

b) Rotating frame behavior of \mathbf{M}



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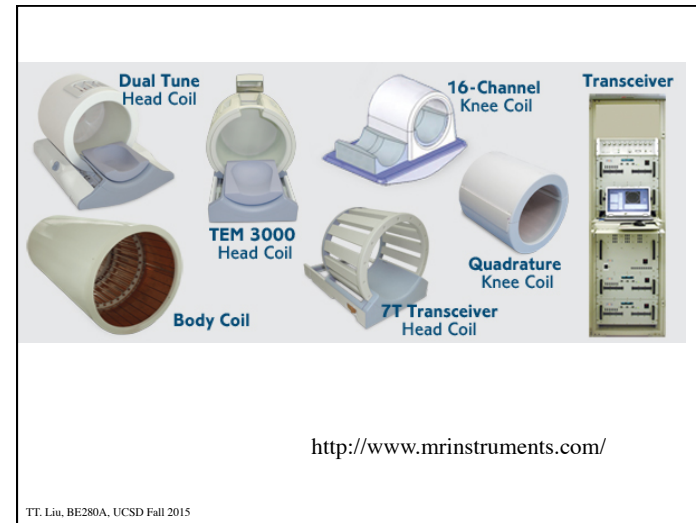
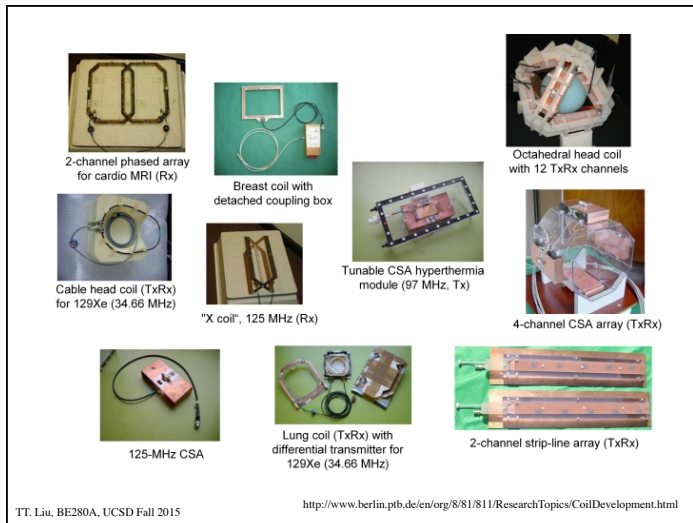
<http://www.eecs.umich.edu/%7EdnohBME516/>



$$\begin{aligned} \mathbf{B}_1(t) &= 2B_1(t)\cos(\omega t)\mathbf{i} \\ &= B_1(t)(\cos(\omega t)\mathbf{i} - \sin(\omega t)\mathbf{j}) + B_1(t)(\cos(\omega t)\mathbf{i} + \sin(\omega t)\mathbf{j}) \end{aligned}$$

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Nishimura 1996



Precession

Analogous to motion of a gyroscope
Precesses at an angular frequency of

$$\omega = \gamma \mathbf{B}$$

This is known as the **Larmor** frequency.

$$\frac{d\boldsymbol{\mu}}{dt} = \boldsymbol{\mu} \times \gamma \mathbf{B}$$

Movement of a Gyroscope
without
External Forces

Concept:
Hermann Härtel

Computer Graphics:
Jan Paul

http://www.astrophysik.uni-kiel.de/~haertel/mpeg_c/gyros_free.mpg

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Rotating Frame Bloch Equation

$$\frac{d\mathbf{M}_{rot}}{dt} = \mathbf{M}_{rot} \times \gamma \mathbf{B}_{eff}$$

$$\mathbf{B}_{eff} = \mathbf{B}_{rot} + \frac{\omega_{rot}}{\gamma}; \quad \omega_{rot} = \begin{bmatrix} 0 \\ 0 \\ -\omega \end{bmatrix}$$

Note: we use the RF frequency to define the rotating frame. If this RF frequency is on-resonance, then the main B_0 field doesn't cause any precession in the rotating frame. However, if the RF frequency is off-resonance, then there will be a net precession in the rotating frame that is give by the difference between the RF frequency and the local Larmor frequency.

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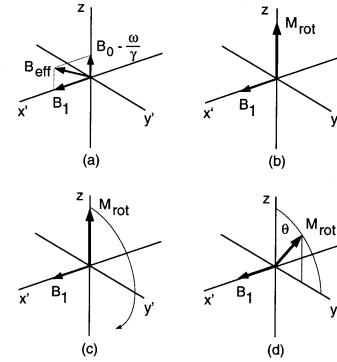
Let $\mathbf{B}_{rot} = B_1(t)\mathbf{i} + B_0\mathbf{k}$

$$\begin{aligned} \mathbf{B}_{eff} &= \mathbf{B}_{rot} + \frac{\omega_{rot}}{\gamma} \\ &= B_1(t)\mathbf{i} + \left(B_0 - \frac{\omega}{\gamma}\right)\mathbf{k} \end{aligned}$$

If $\omega = \omega_0$
 $= \gamma B_0$

Then $\mathbf{B}_{eff} = B_1(t)\mathbf{i}$

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Flip angle

$$\theta = \int_0^\tau \omega_1(s) ds$$

where

$$\omega_1(t) = \gamma B_1(t)$$

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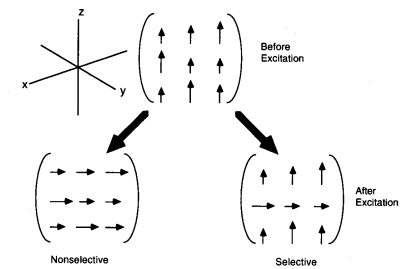
Nishimura 1996

Example

$\tau = 400 \mu\text{sec}; \theta = \pi/2$

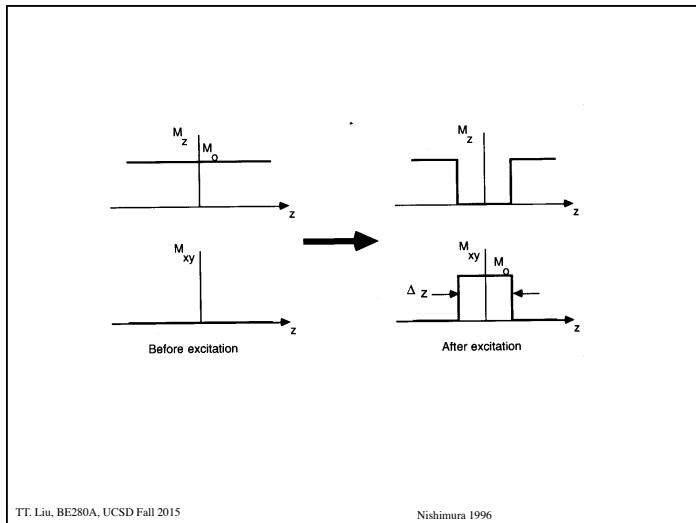
$$B_1 = \frac{\theta}{\gamma\tau} = \frac{\pi/2}{2\pi(4257\text{Hz/G})(400e-6)} = 0.1468 \text{ G}$$

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Nishimura 1996



Let $\mathbf{B}_{rot} = B_1(t)\mathbf{i} + (B_0 + \gamma G_z z)\mathbf{k}$

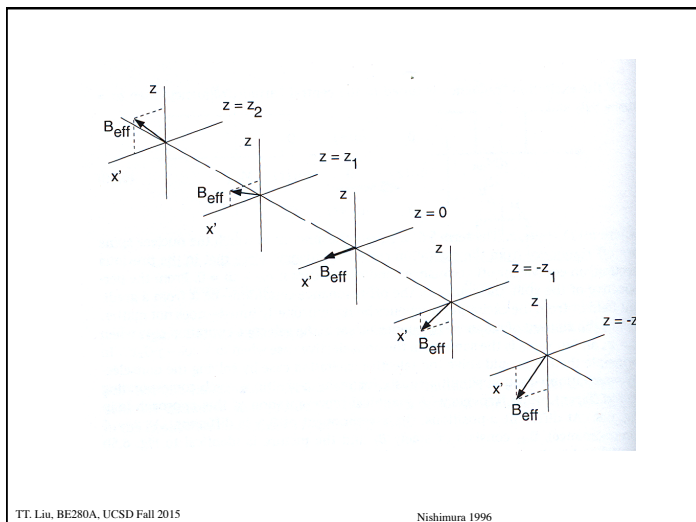
$$\mathbf{B}_{eff} = \mathbf{B}_{rot} + \frac{\omega_{rot}}{\gamma}$$

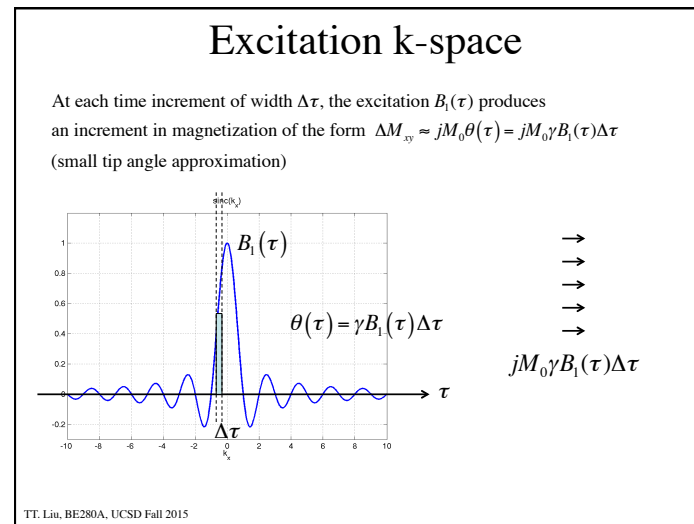
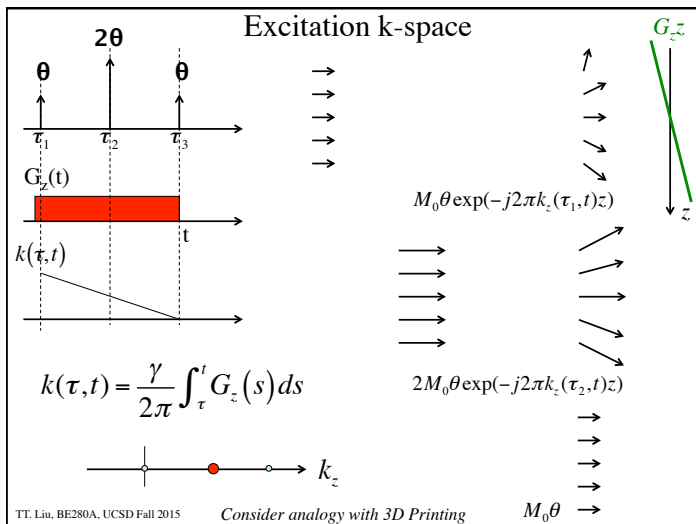
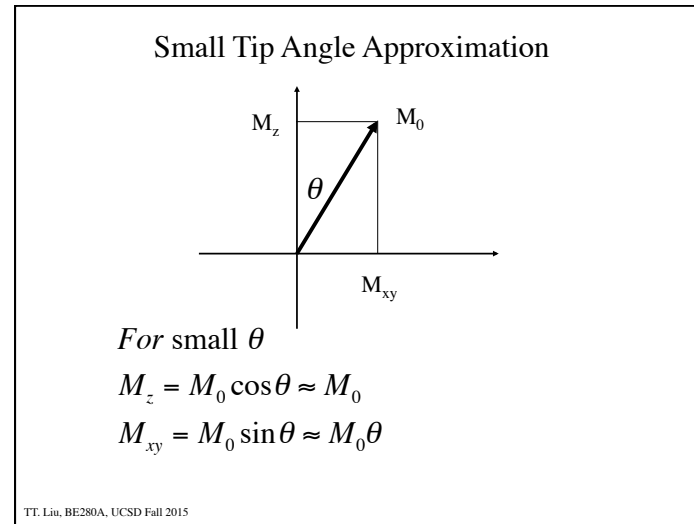
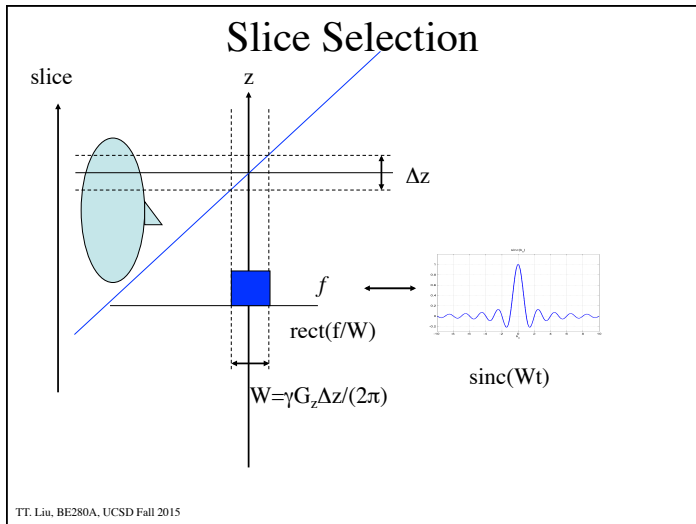
$$= B_1(t)\mathbf{i} + \left(B_0 + \gamma G_z z - \frac{\omega}{\gamma} \right) \mathbf{k}$$

If $\omega = \omega_0$

$$\mathbf{B}_{eff} = B_1(t)\mathbf{i} + (\gamma G_z z)\mathbf{k}$$

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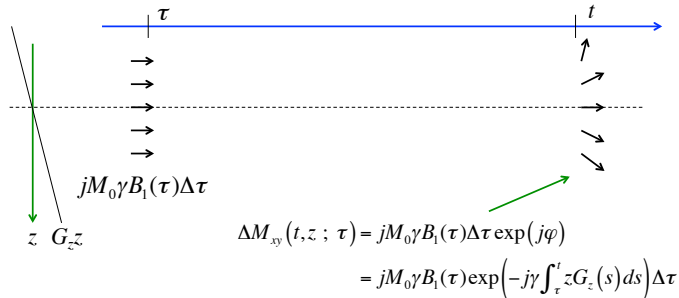




Excitation k-space

In the presence of a gradient, this will accumulate phase of the form $\varphi = -\gamma \int_{\tau}^t z G_z(s) ds$, such that the incremental magnetization at time t is

$$\Delta M_{xy}(t, z; \tau) = jM_0 \gamma B_1(\tau) \exp\left(-j\gamma \int_{\tau}^t z G_z(s) ds\right) \Delta\tau$$



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Excitation k-space

Integrating over all time increments $d\tau$, we obtain

$$M_{xy}(t, z) = jM_0 \int_{-\infty}^t \gamma B_1(\tau) \exp\left(-j\gamma \int_{\tau}^t z G_z(s) ds\right) d\tau$$

$$= jM_0 \int_{-\infty}^t \gamma B_1(\tau) \exp(-j2\pi k(\tau, t)z) d\tau$$

where $k(\tau, t) = \frac{\gamma}{2\pi} \int_{\tau}^t G_z(s) ds$

This has the form of a Fourier transform, where we are integrating the contributions of the field $B_1(\tau)$ at the k-space point $k(\tau, t)$.

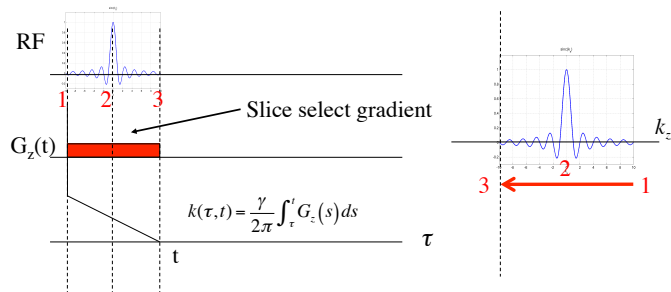
For a historical perspective see <http://www.sciencedirect.com/science/article/pii/S1090780711002655>

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Excitation k-space

$$M_{xy}(t, z) = jM_0 \int_{-\infty}^t \gamma B_1(\tau) \exp(-j2\pi k(\tau, t)z) d\tau$$

This has the form of a Fourier transform, where we are integrating the contributions of the field $B_1(\tau)$ at the k-space point $k(\tau, t)$.

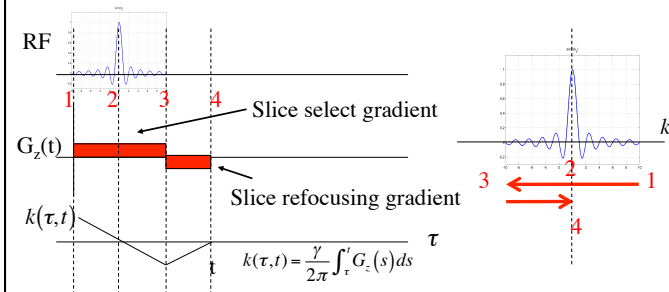


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Refocusing

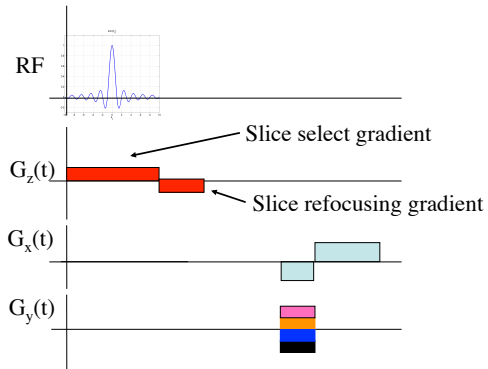
$$M_{xy}(t, z) = jM_0 \int_{-\infty}^t \gamma B_1(\tau) \exp(-j2\pi k(\tau, t)z) d\tau$$

This has the form of a Fourier transform, where we are integrating the contributions of the field $B_1(\tau)$ at the k-space point $k(\tau, t)$.



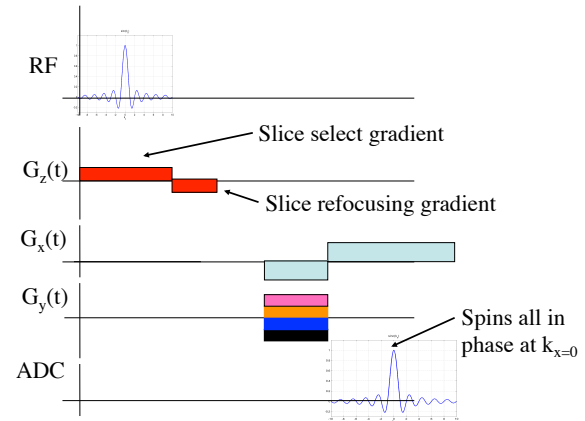
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Slice Selection



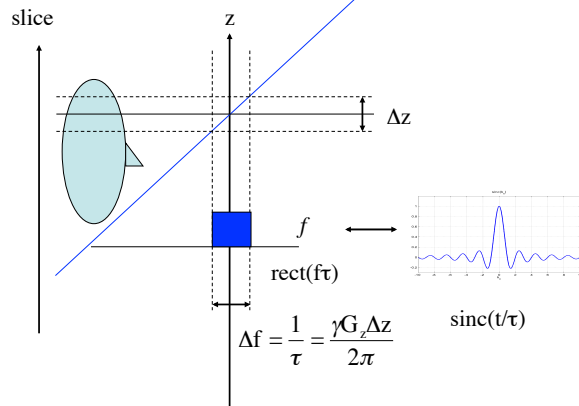
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Gradient Echo

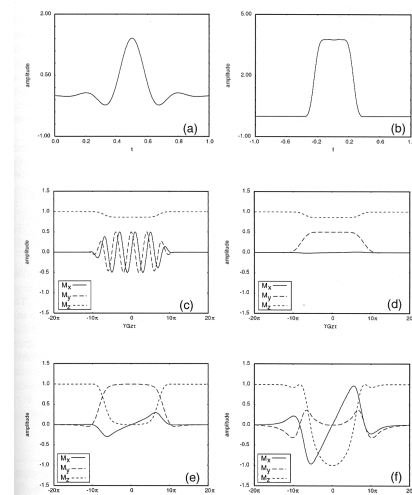


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Slice Selection



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Nishimura 1996

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Example

$$M_{xy}(x) = M_0 \cos(4\pi x)$$

$$F(M_{xy}(x)) = \frac{M_0}{2} (\delta(k_x - 2) + \delta(k_x + 2))$$

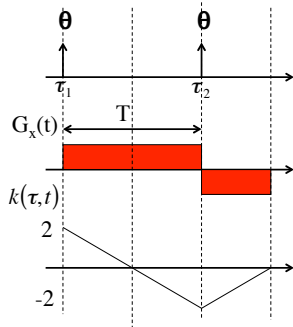
$$g_{\max} = 4 \text{ G/cm}$$

$$\frac{\gamma}{2\pi} g_{\max} T = 4 \text{ cm}^{-1}; \quad T = 235 \text{ } \mu\text{sec}$$

with small tip angle approximation $\rightarrow \theta = \frac{1}{2}$

$$\text{Compare with } \sin\left(\frac{\pi}{6}\right) = \frac{1}{2} \rightarrow \theta = \frac{\pi}{6} = 0.5236$$

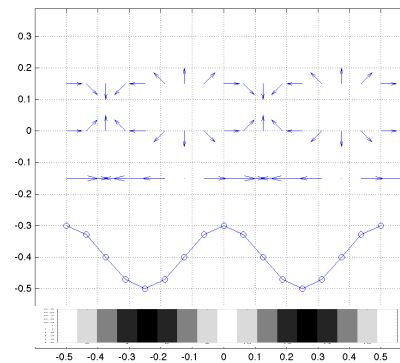
Question: Should we use $\theta = \frac{\pi}{4}$ instead?



Exercise: Sketch the quiver diagrams corresponding to the contributions of the two RF pulses and show that they produce the desired pattern.

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Exercise: Sketch the quiver diagrams corresponding to the contributions of the two RF pulses and show that they produce the desired pattern. (Patterns shown below scaled for display purposes)



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Multi-dimensional Excitation k-space

$$M_{xy}(t, \mathbf{r}) = jM_0 \int_{-\infty}^t \omega_1(\tau) \exp\left(-j\gamma \int_{\tau}^t \mathbf{G}(s) \cdot \mathbf{r} ds\right) d\tau$$

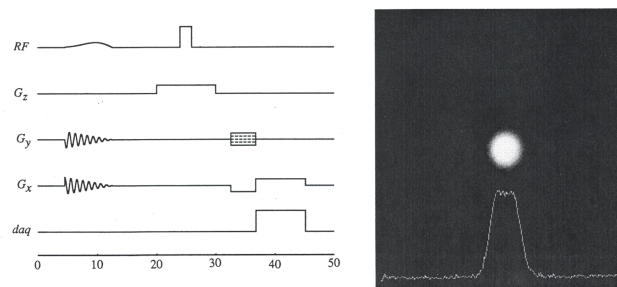
$$= jM_0 \int_{-\infty}^t \omega_1(\tau) \exp(j2\pi \mathbf{k}(\tau) \cdot \mathbf{r}) d\tau$$

$$\text{where } \mathbf{k}(\tau) = -\frac{\gamma}{2\pi} \int_{\tau}^t \mathbf{G}(t') d\tau'$$

Pauly et al 1989

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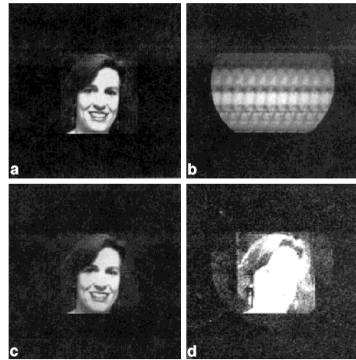
Excitation k-space



Pauly et al 1989

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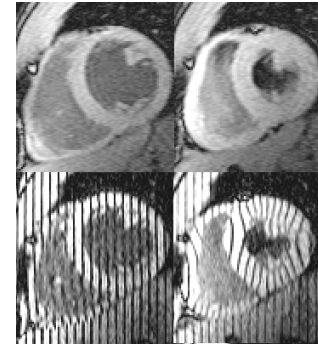
Excitation k-space



Panych MRM 1999

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Cardiac Tagging



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