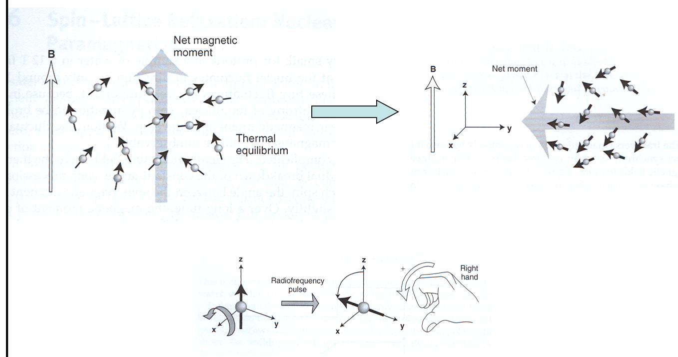
Bioengineering 280A
Principles of Biomedical Imaging

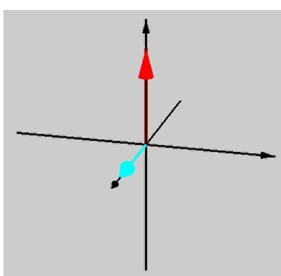
Fall Quarter 2015
MRI Lecture 6

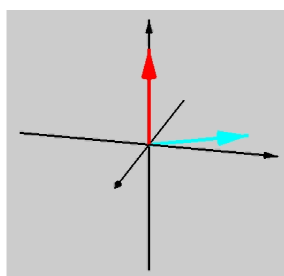
RF Excitation



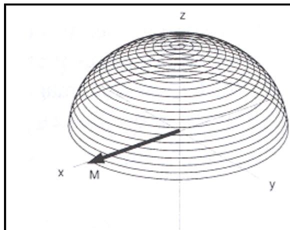
From Levitt, Spin Dynamics, 2001

RF Excitation



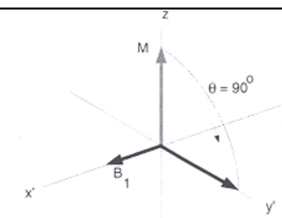


http://www.eecs.umich.edu/%7EdnollBME516/

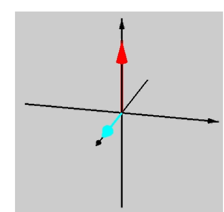


a) Laboratory frame behavior of **M**

Images & caption: Nishimura, Fig. 3.3



b) Rotating frame behavior of **M**



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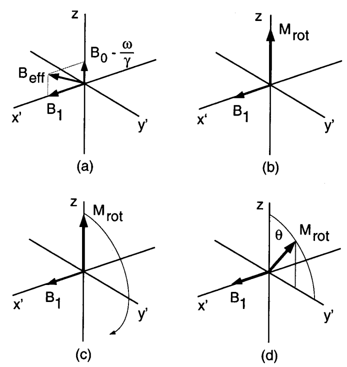

Flip angle

$$\theta = \int_0^{\tau} \omega_1(s)ds$$

where

$$\omega_1(t) = \gamma B_1(t)$$

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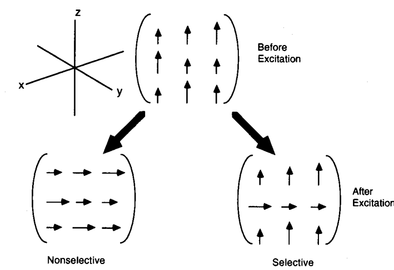
Nishimura 1996



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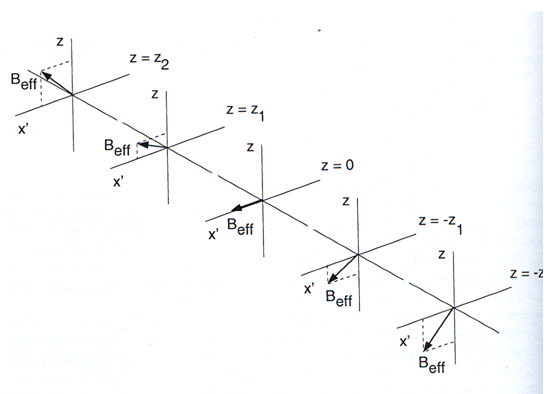
Nishimura 1996



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Nishimura 1996

https://www.youtube.com/watch?v=kODOL-QBzSM

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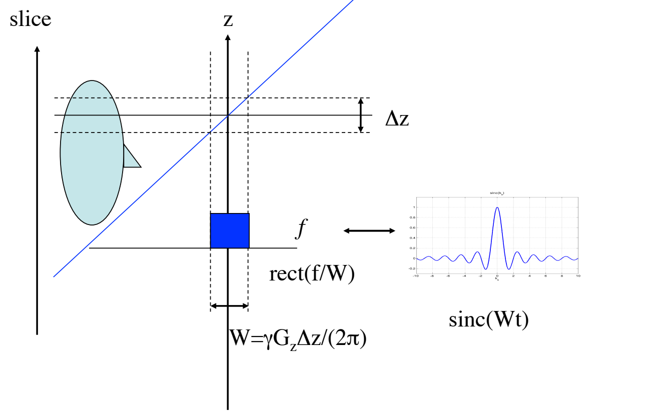
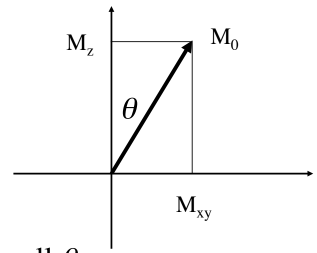
Slice Selection



Small Tip Angle Approximation

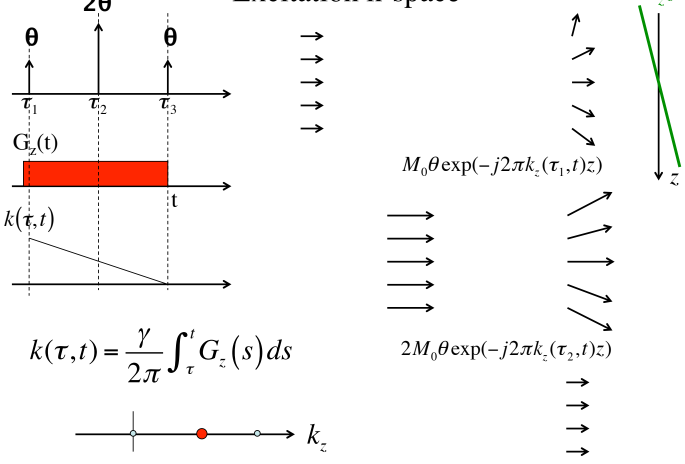


For small θ

$$M_z = M_0 \cos\theta \approx M_0$$

$$M_{xy} = M_0 \sin\theta \approx M_0\theta$$

Excitation k-space

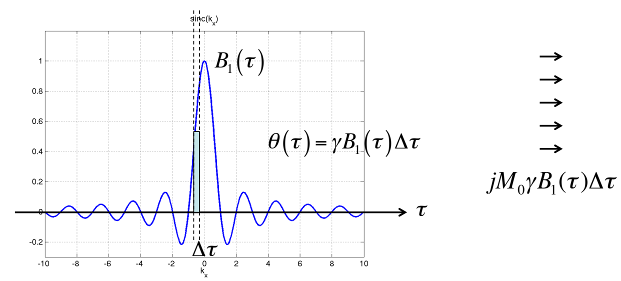


$$k(\tau,t) = \frac{\gamma}{2\pi}\int_{\tau}^{t} G_z(s)\,ds$$

Consider analogy with 3D Printing

Excitation k-space

At each time increment of width $\Delta\tau$, the excitation $B_1(\tau)$ produces an increment in magnetization of the form $\Delta M_{xy} \approx jM_0\theta(\tau) = jM_0\gamma B_1(\tau)\Delta\tau$ (small tip angle approximation)

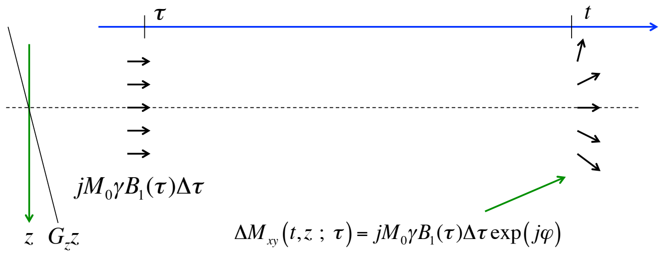


Excitation k-space

In the presence of a gradient, this will accumulate phase of the form

$\varphi = -\gamma \int_\tau^t z G_z(s)\,ds$, such that the incremental magnetization at time t is

$$\Delta M_{xy}(t,z\,;\,\tau) = jM_0 \gamma B_1(\tau) \exp\left(-j\gamma \int_\tau^t z G_z(s)\,ds\right)\Delta\tau$$



$$\Delta M_{xy}(t,z\,;\,\tau) = jM_0\gamma B_1(\tau)\Delta\tau \exp(j\varphi)$$
$$= jM_0\gamma B_1(\tau)\exp\left(-j\gamma\int_\tau^t z G_z(s)\,ds\right)\Delta\tau$$

Excitation k-space

Integrating over all time increments $d\tau$, we obtain

$$M_{xy}(t,z) = jM_0 \int_{-\infty}^t \gamma B_1(\tau)\exp\left(-j\gamma\int_\tau^t z G_z(s)\,ds\right)d\tau$$
$$= jM_0 \int_{-\infty}^t \gamma B_1(\tau)\exp\left(-j2\pi k(\tau,t)z\right)d\tau$$

where $k(\tau,t) = \frac{\gamma}{2\pi}\int_\tau^t G_z(s)\,ds$

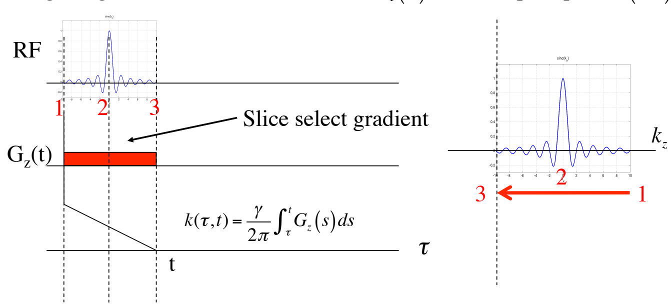
This has the form of a Fourier transform, where we are integrating the contributions of the field $B_1(\tau)$ at the k-space point $k(\tau,t)$.

For a historical perspective see
http://www.sciencedirect.com/science/article/pii/S1090780711002655

Excitation k-space

$$M_{xy}(t,z) = jM_0 \int_{-\infty}^t \gamma B_1(\tau)\exp\left(-j2\pi k(\tau,t)z\right)d\tau$$

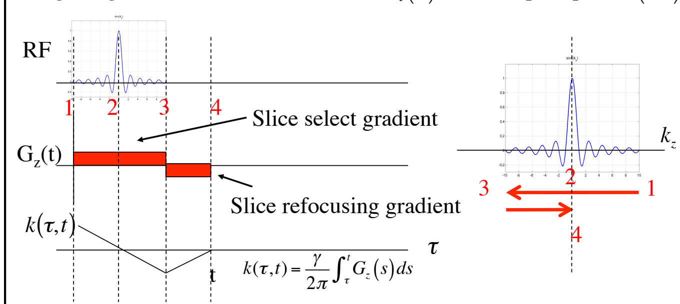
This has the form of a Fourier transform, where we are integrating the contributions of the field $B_1(\tau)$ at the k-space point $k(\tau,t)$.



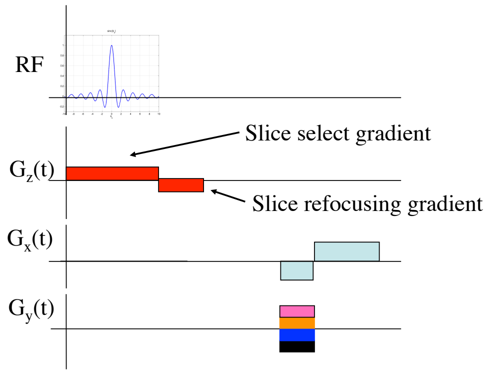
Refocusing

$$M_{xy}(t,z) = jM_0 \int_{-\infty}^t \gamma B_1(\tau)\exp\left(-j2\pi k(\tau,t)z\right)d\tau$$

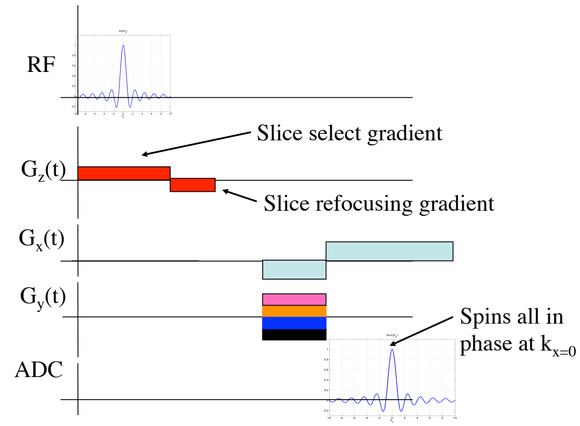
This has the form of a Fourier transform, where we are integrating the contributions of the field $B_1(\tau)$ at the k-space point $k(\tau,t)$.



Slice Selection



Gradient Echo



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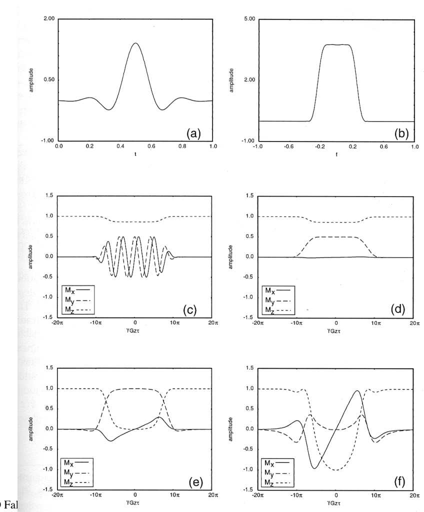

Nishimura 1996

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Example

$M_{xy}(x) = M_0 \cos(4\pi x)$

$F\left(M_{xy}(x)\right) = \frac{M_0}{2}\left(\delta(k_x - 2) + \delta(k_x + 2)\right)$

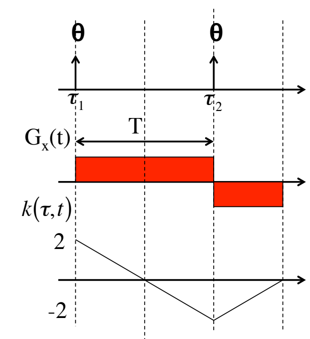
$g_{\max} = 4\ G/cm$

$\frac{\gamma}{2\pi} g_{\max} T = 4\ \text{cm}^{-1};\ \ \text{T} = 235\ \mu\text{sec}$

with small tip angle approximation --> $\theta = \frac{1}{2}$

Compare with $\sin\left(\frac{\pi}{6}\right) = \frac{1}{2} \rightarrow \theta = \frac{\pi}{6} = 0.5236$

Question: Should we use $\theta = \frac{\pi}{4}$ instead?



Exercise: Sketch the quiver diagrams corresponding to the contributions of the two RF pulses and show that they produce the desired pattern.

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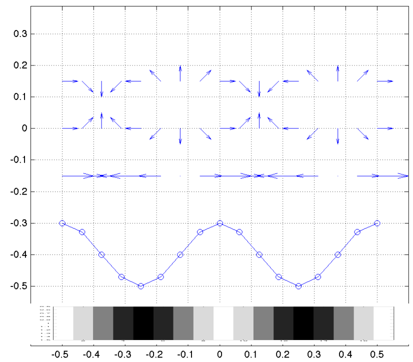
Exercise: Sketch the quiver diagrams corresponding to the contributions of the two RF pulses and show that they produce the desired pattern. (Patterns shown below scaled for display purposes)



Slice Selection Problem

Consider a desired slice profile of the form $m(z) = M_0 rect(z/(10mm))$.

You are given an RF pulse of the form $p(t) = A \cdot \text{sinc}\left(\frac{t}{T}\right)$

where $T = 400\ \mu\text{sec}$

(1)What amplitude gradient should you use to achieve the desired slice profile?
HINT : Think about where the first zero in k_z space must appear. Then think about what gradient is needed so that the first zero in the RF occurs at the desired location in k-space. An alternate approach is to consider the frequency range of the spins that need to be excited within the slice and also consider the bandwidth of the RF pulse.

(2) What should the amplitude A of the RF pulse be?

(3)What happens to the slice profile if you truncate the RF pulse to have a duration of 3.2 ms?

Time-Bandwidth Product (TBW)

$$\text{sinc}(t/\tau)rect\left(\frac{t}{2N\tau}\right) \Rightarrow \tau rect(\tau f) * 2N\tau \text{sinc}(2N\tau f)$$

N = number of zeros in Sinc

Duration $= 2N\tau$

Bandwidth $= \frac{1}{\tau} \quad \Rightarrow \Delta z = \frac{2\pi}{\gamma G_z \tau}$

Transition Width $\approx \frac{1}{2N\tau} \quad \Rightarrow \Delta z' = \frac{2\pi}{\gamma G_z 2N\tau}$

Time – Bandwidth Product (TBW) $= 2N\tau\frac{1}{\tau} = 2N$

also, TBW= $\frac{\text{Bandwidth}}{\text{Transition Width}}$

For a fixed duration pulse, we can increase TBW by increasing the Bandwidth.
(Note : this will also lead to an increase in N).
This will require a higher B1 amplitude and a higher gradient to keep the slice width constant -- note that with higher TBW the physical transition width then decreases.

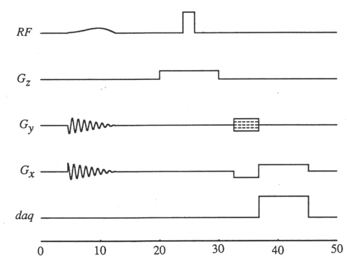
Multi-dimensional Excitation k-space

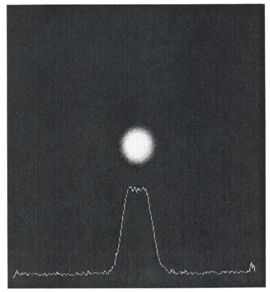
$$M_{xy}(t,\mathbf{r}) = jM_0\int_{-\infty}^{t}\omega_1(\tau)\exp\left(-j\gamma\int_{\tau}^{t}\mathbf{G}(s)\cdot\mathbf{r}ds\right)d\tau$$
$$= jM_0\int_{-\infty}^{t}\omega_1(\tau)\exp\left(j2\pi\mathbf{k}(\tau)\cdot\mathbf{r}\right)d\tau$$

where $\quad \mathbf{k}(\tau) = -\frac{\gamma}{2\pi}\int_{\tau}^{t}\mathbf{G}(t')dt'$

Pauly et al 1989

Excitation k-space





Pauly et al 1989

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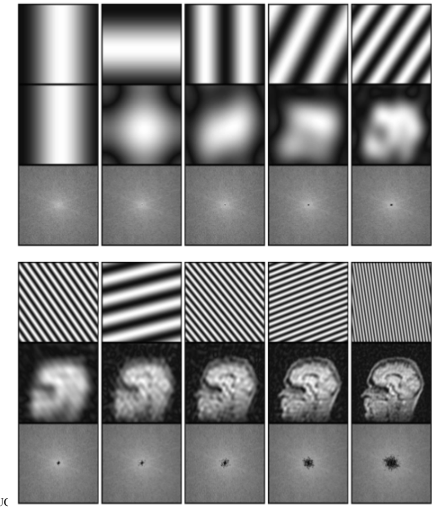

Hanson 2009

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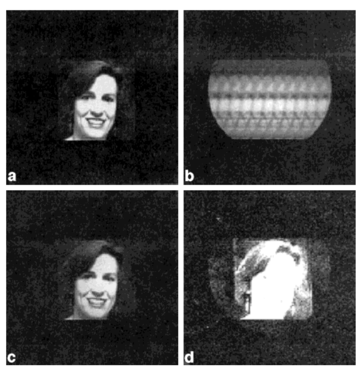
Excitation k-space



Panych MRM 1999

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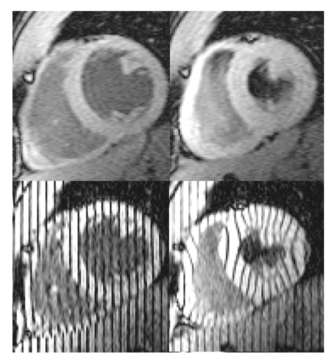
Cardiac Tagging



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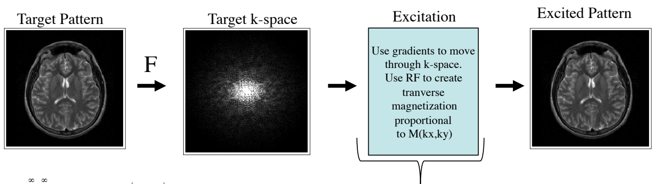
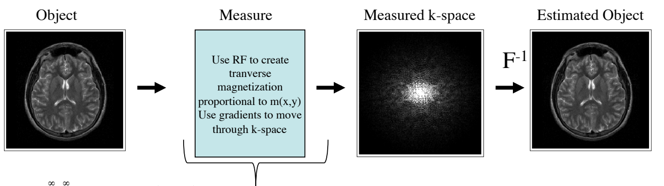
Imaging and Excitation



$\int_{-\infty}^{\infty}\int_{-\infty}^{\infty} M(k_x,k_y)e^{j2\pi(k_x x+k_y y)}dk_x\, dk_y$; integration over k performed incrememtanlly by layering of spins in place



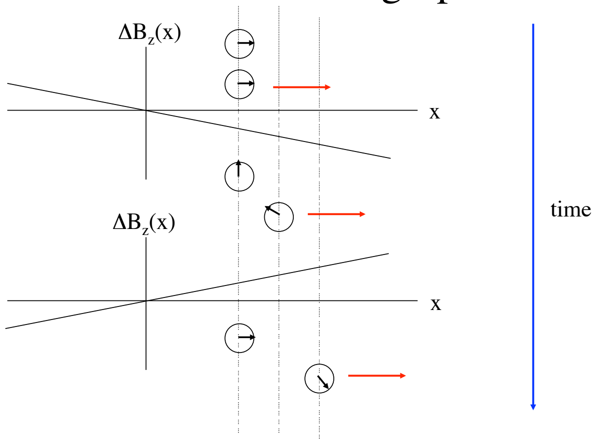
$\int_{-\infty}^{\infty}\int_{-\infty}^{\infty} m(x,y)e^{-j2\pi(k_x x+k_y y)}dx\,dy$; integration over space performed instantaneously by coil

Moving Spins (preview)

So far we have assumed that the spins are not moving (aside from thermal motion giving rise to relaxation), and contrast has been based upon T_1, T_2, and proton density. We were able to achieve different contrasts by adjusting the appropriate pulse sequence parameters.

Biological samples are filled with moving spins, and we can also use MRI to image the movement. Examples: blood flow, diffusion of water in the white matter tracts. In addition, we can also sometimes induce motion into the object to image its mechanical properties, e.g. imaging of stress and strain with MR elastography.

Phase of Moving Spin



Phase of a Moving Spin

$$
\begin{aligned}
\varphi(t) &= -\int_0^t \Delta\omega(\tau)d\tau \\
&= -\int_0^t \gamma\Delta B(\tau)d\tau \\
&= -\int_0^t \gamma\vec{G}(\tau)\cdot\vec{r}(\tau)d\tau \\
&= -\gamma\int_0^t \left[G_x(\tau)x(\tau)+G_y(\tau)y(\tau)+G_z(\tau)z(\tau)\right]d\tau
\end{aligned}
$$

Phase of Moving Spin

Consider motion along the x-axis

$$x(t) = x_0 + vt + \frac{1}{2}at^2$$

$$\begin{aligned}\varphi(t) &= -\gamma\int_0^t G_x(\tau)x(\tau)d\tau \\ &= -\gamma\int_0^t G_x(\tau)\left[x_0 + v\tau + \frac{1}{2}a\tau^2\right]d\tau \\ &= -\gamma\left[x_0\int_0^t G_x(\tau)d\tau + v\int_0^t G_x(\tau)\tau d\tau + \frac{a}{2}\int_0^t G_x(\tau)\tau^2 d\tau\right] \\ &= -\gamma\left[x_0 M_0 + vM_1 + \frac{a}{2}M_2\right]\end{aligned}$$

Phase of Moving Spin

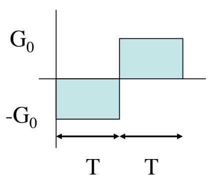
$$\varphi(t) = -\gamma\left[x_0 M_0 + vM_1 + \frac{a}{2}M_2\right]$$

$M_0 = \int_0^t G_x(\tau)d\tau$ Zeroth order moment

$M_1 = \int_0^t G_x(\tau)\tau d\tau$ First order moment

$M_2 = \int_0^t G_x(\tau)\tau^2 d\tau$ Second order moment

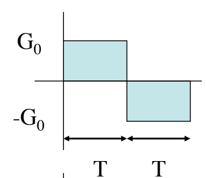
Flow Moment Example



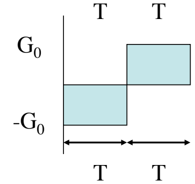
$$M_0 = \int_0^t G_x(\tau)d\tau = 0$$

$$\begin{aligned}M_1 &= \int_0^t G_x(\tau)\tau d\tau \\ &= -\int_0^T G_0\tau d\tau + \int_T^{2T} G_0\tau d\tau \\ &= G_0\left[-\frac{\tau^2}{2}\bigg|_0^T + \frac{\tau^2}{2}\bigg|_T^{2T}\right] \\ &= G_0\left[-\frac{T^2}{2} + \frac{4T^2}{2} - \frac{T^2}{2}\right] = G_0 T^2\end{aligned}$$

Phase Contrast Angiography (PCA)



$$\varphi_1 = -\gamma v_x M_1 = \gamma v_x G_0 T^2$$

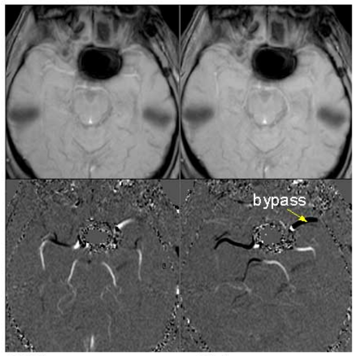


$$\varphi_2 = -\gamma v_x M_1 = -\gamma v_x G_0 T^2$$

$$\Delta\varphi = \varphi_1 - \varphi_2 = 2\gamma v_x G_0 T^2$$

$$v_x = \frac{\Delta\varphi}{2G_0 T^2}$$

PCA example



White = Flow direction AP (↓)

White = Flow direction RL (→)

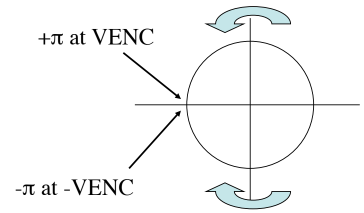
http://www.medical.philips.com/main/products/mri/assets/images/case_of_week/cotw_51_s5.jpg

Aliasing in PCA

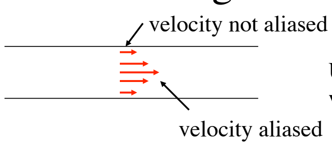
Define VENC as the velocity at at which the phase is 180 degrees.

$$VENC \equiv \frac{\pi}{\gamma G_0 T^2}$$

Because of phase wrapping the velocity of spins flowing faster than VENC is ambiguous.



Aliasing Solutions



Use data from regions with slower flow

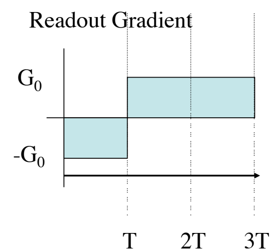
Use multiple VENC values so that the phase differences are smaller than π radians.

$$\varphi_1 = \pi \frac{v_x}{VENC_1}$$

$$\varphi_2 = \pi \frac{v_x}{VENC_2}$$

$$\varphi_1 - \varphi_2 = \pi v_x \left(\frac{1}{VENC_1} - \frac{1}{VENC_2} \right)$$

Flow Artifacts



During readout moving spins within the object will accumulate phase that is in addition to the phase used for imaging. This leads to

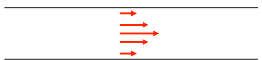
1) Net phase at echo time TE = 2T.
2) An apparent shift in position of the object.
3) Blurring of the object due to a quadratic phase term.

Flow Artifacts

Plug Flow

All moving spins in the voxel experience the same phase shift at echo time.

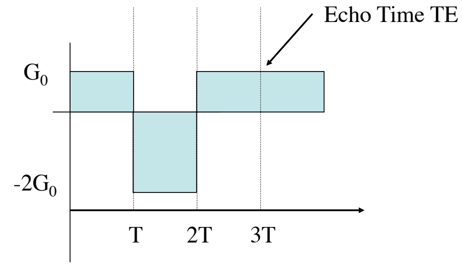
Laminar Flow



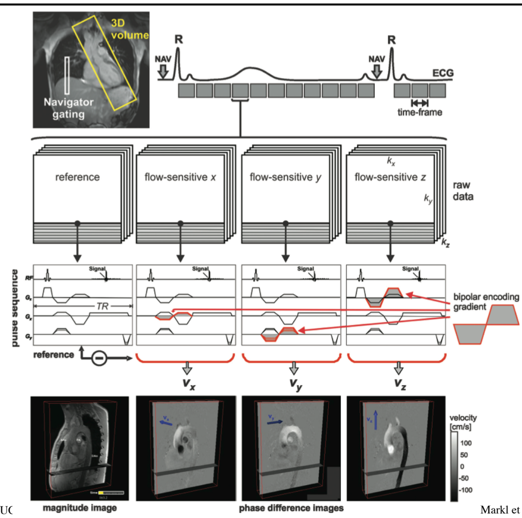
Spins have different phase shifts at echo time. The dephasing causes the cancelation and signal dropout.

Flow Compensation

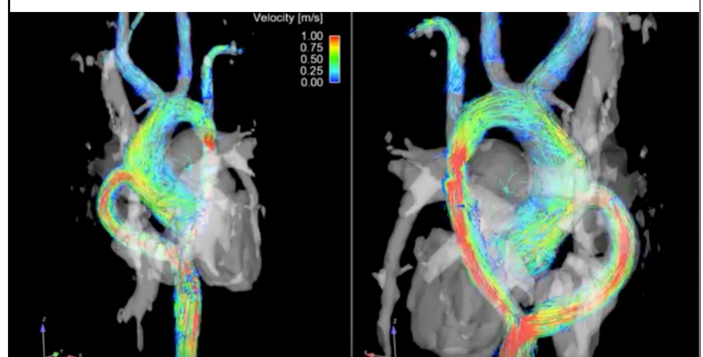
Readout Gradient



At TE both the first and second order moments are zero, so both stationary and moving spins have zero net phase.



Markl et al JMRI 2012



https://www.youtube.com/watch?v=1ORpeB6j0gc

Velocity k-space

A bipolar gradient introduces a phase modulation across velocities of the form $\varphi(v_x) = -\gamma v_x G_0 T^2$

The MRI signal (with no spatial encoding) acquired across a volume of spins with varying velocities is:

$$\begin{aligned} M(k_{v_x}) &= \int_{-\infty}^{\infty} m(v_x) e^{j\varphi(v_x)} dv_x \\ &= \int_{-\infty}^{\infty} m(v_x) e^{-j\gamma v_x G_0 T^2} dv_x \\ &= \int_{-\infty}^{\infty} m(v_x) e^{-j2\pi k_{v_x} v_x} dv_x \\ &= F\left[m(v_x)\right] \text{ with } k_{v_x} = \frac{\gamma}{2\pi} G_0 T^2 \end{aligned}$$

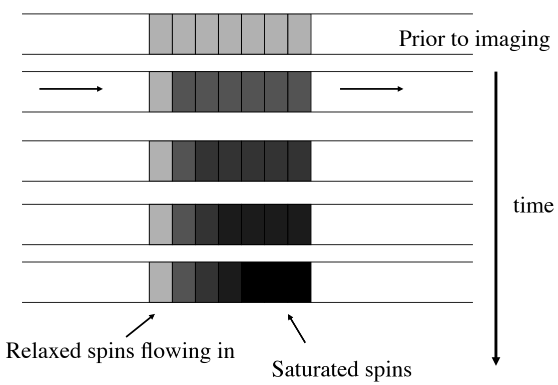
By making measurements with bipolar gradients of varying amplitudes/durations and taking the inverse transform of the measurements, we can obtain the velocity distribution.

Velocity k-space

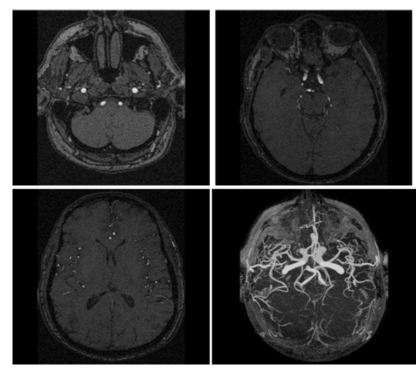
$$M(k_x, k_{v_x}) = \int_{-\infty}^{\infty}\int_{-\infty}^{\infty} m(x, v_x) e^{-j2\pi k_x x} e^{-j2\pi k_{v_x} v_x} dx dv_x$$

In addition, we can apply imaging gradients so that we can eventually obtain the velocity distribution at each point in space. A full k-space acqusition would then yield 6 dimensions -- 3 spatial dimensions and 3 velocity dimensions.

Inflow Effect



Time of Flight Angiography



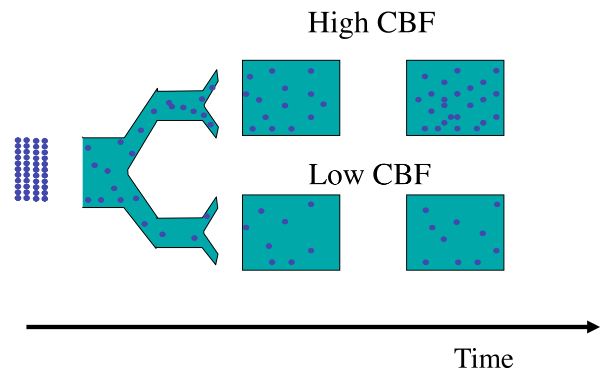
Cerebral Blood Flow (CBF)

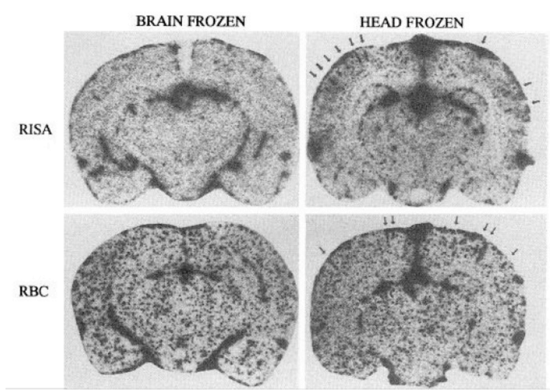
CBF = Perfusion

= Rate of delivery of arterial blood to a capillary bed in tissue.

Units: $\frac{\text{(ml of Blood)}}{\text{(100 grams of tissue)(minute)}}$

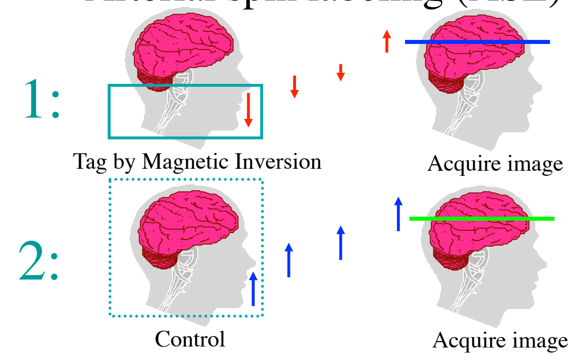
Typical value is 60 ml/(100g-min) or 60 ml/(100 ml-min) = 0.01 s^{-1}, assuming average density of brain equals 1 gm/ml





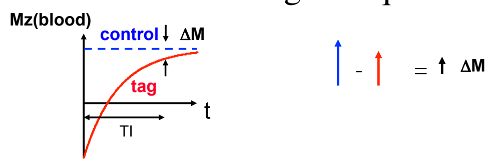
Bereczki et al 1992

Arterial spin labeling (ASL)



Control - Tag = $\Delta M \propto$ CBF

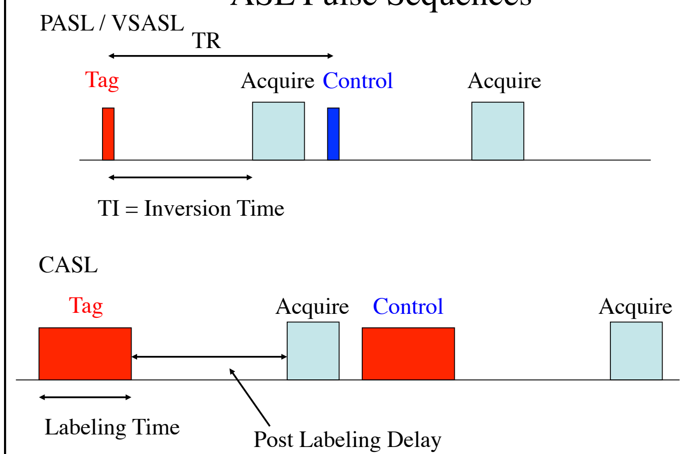
ASL Signal Equation



$$\Delta M = CBF \cdot A_{eff}$$

A_{eff} is the effective area of the arterial bolus. It depends on both physiology and pulse sequence parameters.

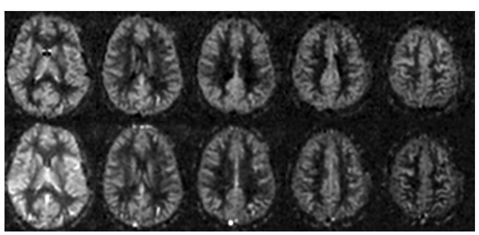
ASL Pulse Sequences



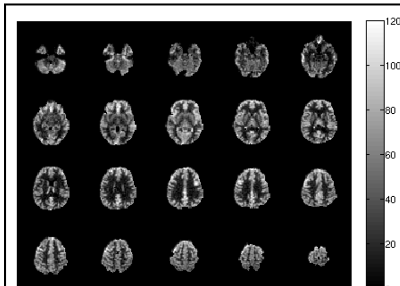
Multislice CASL and PICORE

CASL

PICORE
QUIPSS II

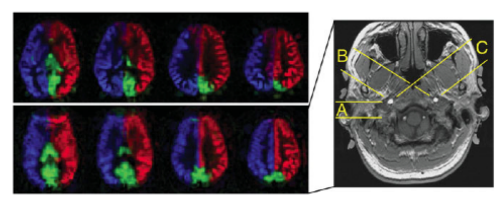


Credit: E. Wong

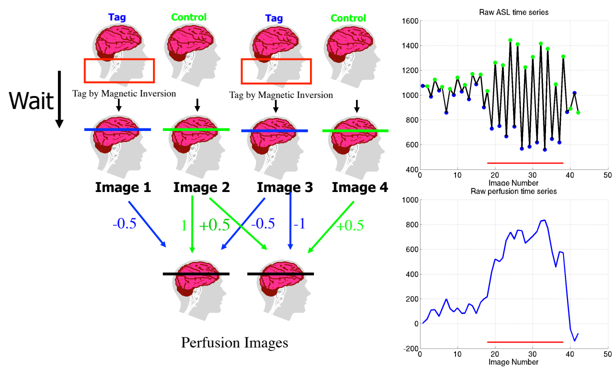


Whole brain non-invasive measures of Cerebral Blood Flow obtained with arterial spin labeling (ASL) MRI (Courtesy of D. Shin)

Vascular territory imaging using vessel-encoded ASL (Wong 2007)



ASL Time Series



TT. Liu, BE280A, UCSD Fall 2015