Bioengineering 280A
Principles of Biomedical Imaging

Fall Quarter 2015
X-Rays Lecture 2

Magnification of Object
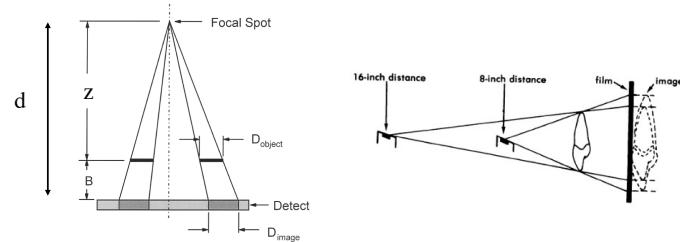
$$M(z) = \frac{d}{z}$$

$$= \frac{\text{Source to Image Distance (SID)}}{\text{Source to Object Distance (SOD)}}$$
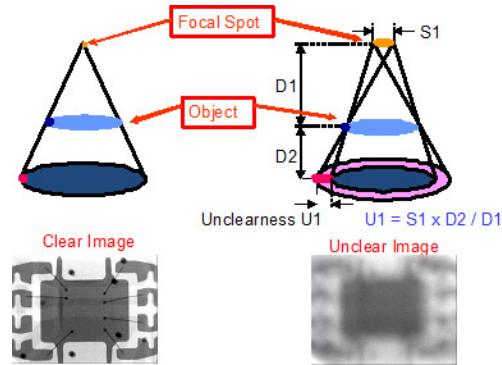
Source magnification

U1 = S1 x D2 / D1

Clear Image   Unclear Image

Source magnification

$$\frac{D_{image}}{D_{focal}} = \frac{d-z}{z}$$

$$m(z) = -\frac{d-z}{z} = -\frac{B}{A}$$

$$= 1 - M(z)$$

Bushberg et al 2001
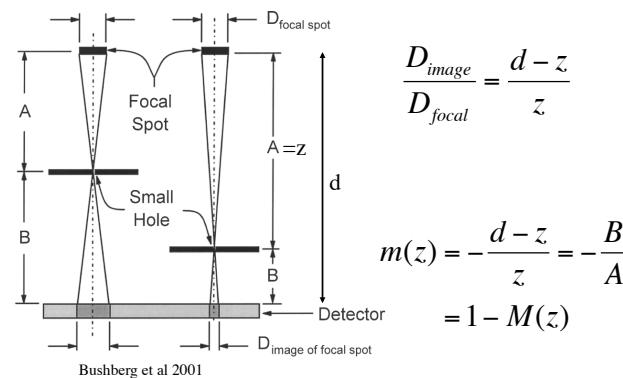
Rectangle Function

$$\Pi(x) = \begin{cases} 0 & |x| > 1/2 \\ 1 & |x| \le 1/2 \end{cases}$$
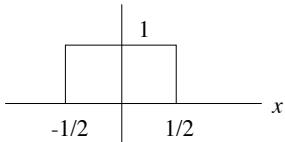
Also called rect(x)

$$\Pi(x, y) = \Pi(x)\Pi(y)$$
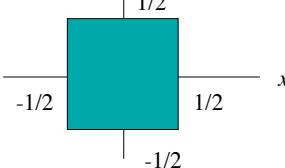
Dirac Delta Function

Notation :

$\delta(x)$ - 1D Dirac Delta Function

$\delta(x, y)$ or $^2\delta(x, y)$ - 2D Dirac Delta Function

$\delta(x, y, z)$ or $^3\delta(x, y, z)$ - 3D Dirac Delta Function

$\delta(\vec{r})$ - N Dimensional Dirac Delta Function
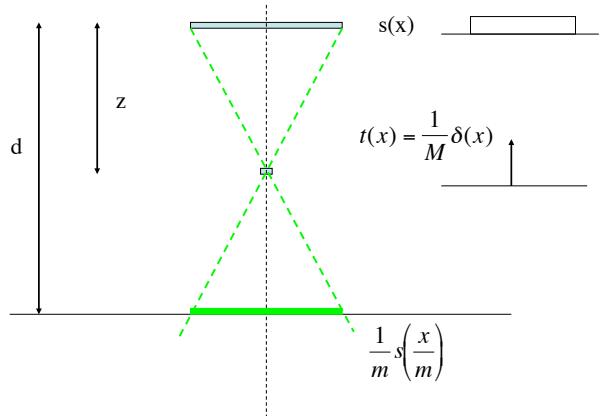
X-Ray Imaging

s(x)

$$t(x) = \frac{1}{M}\delta(x)$$

$$\frac{1}{m}s\left(\frac{x}{m}\right)$$

(a) 10 cm

z

d

Assume z=d/2

(b) 10 cm

z

d

Assume z = .9d

(c) 10 cm

z

d

Assume z=0.1d

(d) 10 cm

z

d

Assume z = .99d

2

Slide (top-left)

(a)   (b)

10 cm   10 cm

z   z

5 cm   5 cm

d   d

Assume z=d/2   Assume z=d/2

pollEv.com/be280a

Slide (top-right)

X-Ray Imaging

s(x)

z

$$t(x) = \frac{1}{M}\delta(x - x_0)$$

d

x_0

x_0

$$M(z) = \frac{d}{z}; \quad m(z) = -\frac{d-z}{z}$$

Mx_0

$$\frac{1}{m}s\left(\frac{x - Mx_0}{m}\right)$$

Slide (bottom-left)

X-Ray Imaging

$$s(x) = rect(x/10)$$

z

d

$$t(x) = rect(x/10)$$

$$M(z) = \frac{d}{z}; \quad m(z) = -\frac{d-z}{z} \qquad \frac{1}{m}s\left(\frac{x}{m}\right) * t\left(\frac{x}{M}\right)$$

Slide (bottom-right)

Signals and Images

Discrete-time/space signal /image: continuous valued function with a discrete time/space index, denoted as *s[n]* for 1D, *s[m,n]* for 2D , etc.

n

n

m

Continuous-time/space signal /image: continuous valued function with a continuous time/space index, denoted as *s(t)* or *s(x)* for 1D, *s(x,y)* for 2D, etc.

t

y

x

3
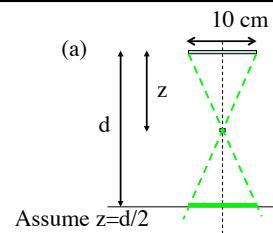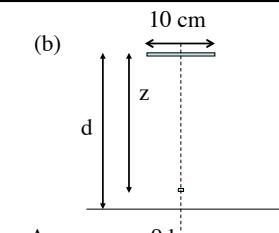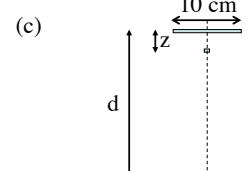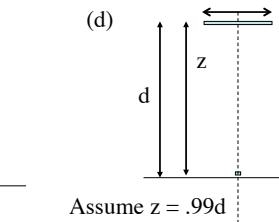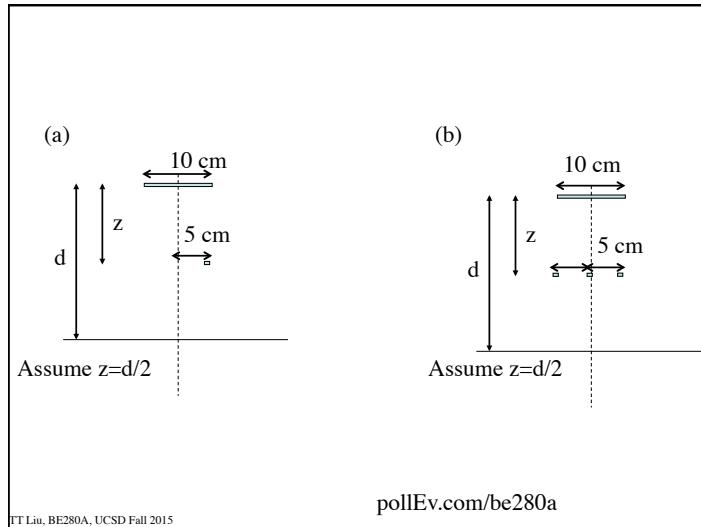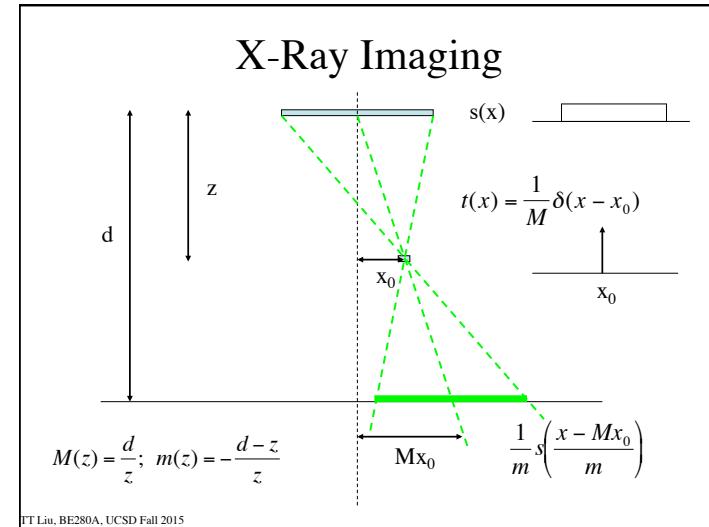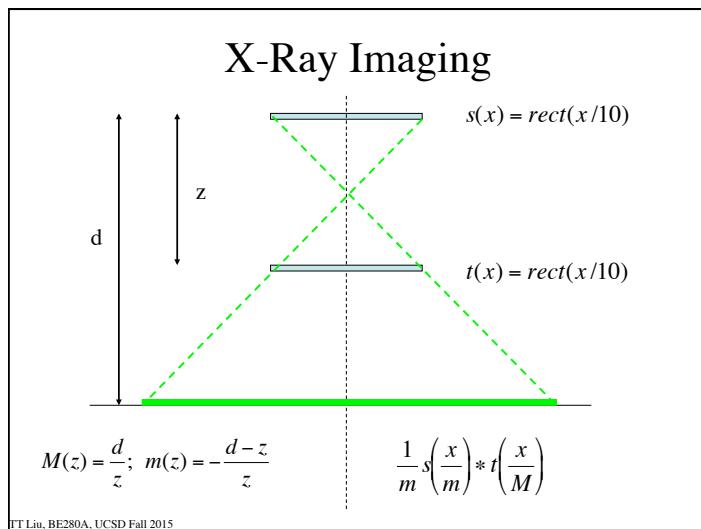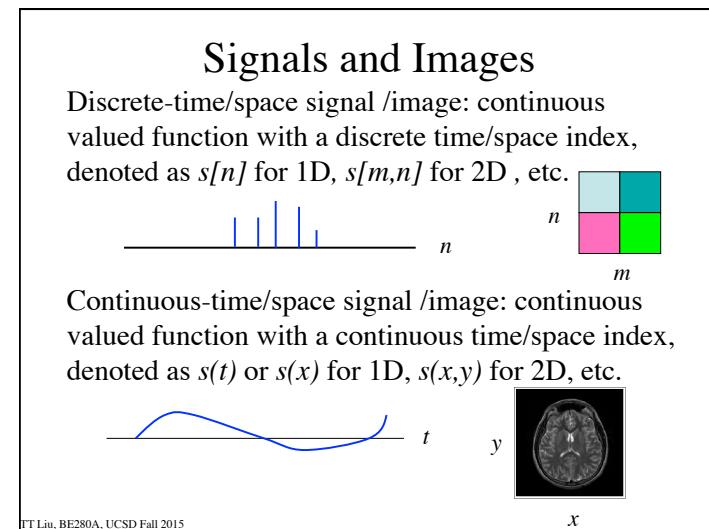
Kronecker Delta Function

$$\delta[n] = \begin{cases} 1 & \text{for } n = 0 \\ 0 & otherwise \end{cases}$$

δ[n]

n

0

δ[n-2]

n

0
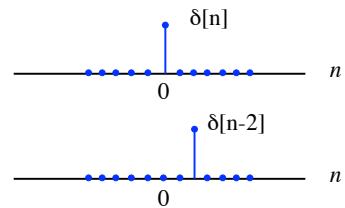
Kronecker Delta Function

$$\delta[m,n] = \begin{cases} 1 & \text{for } m = 0, n = 0 \\ 0 & otherwise \end{cases}$$

δ[m,n]   δ[m-2,n]

δ[m,n-2]   δ[m-2,n-2]
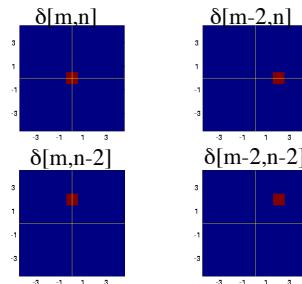
Discrete Signal Expansion

$$g[n] = \sum_{k=-\infty}^{\infty} g[k]\delta[n-k]$$

$$g[m,n] = \sum_{k=-\infty}^{\infty}\sum_{l=-\infty}^{\infty} g[k,l]\delta[m-k,n-l]$$

g[n]

n

δ[n]

n

0

-δ[n-1]

n

0

1.5δ[n-2]

n

0

2D Signal

a	b
c	d

=

a	0
0	0

+

0	b
0	0

+

0	0
c	0

+

0	0
0	d

4

Image Decomposition

c	d
a	b

$=$

c
1	0
0	0

$+d$
0	1
0	0

$+$

a
0	0
1	0

$+b$
0	0
0	1

$$g[m,n] = a\delta[m,n] + b\delta[m,n-1] + c\delta[m-1,n] + d\delta[m-1,n-1]$$

$$= \sum_{k=0}^{1}\sum_{l=0}^{1} g[k,l]\delta[m-k,n-l]$$

3	4	5
6	7	8
1	2	3
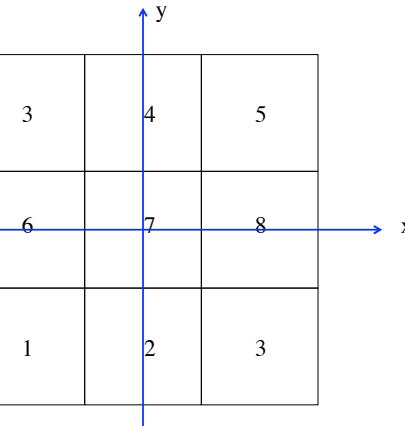
Example: Write in signal expansion form

1D Dirac Delta Function

$\delta(x) = 0$ when $x \neq 0$ and $\int_{-\infty}^{\infty}\delta(x)dx = 1$

Can interpret the integral as a limit of the integral of an ordinary function that is shrinking in width and growing in height, while maintaining a constant area. For example, we can use a shrinking rectangle function

such that $\int_{-\infty}^{\infty}\delta(x)dx = \lim_{\tau \to 0}\int_{-\infty}^{\infty}\tau^{-1}\Pi(x/\tau)dx$.

$\tau \to 0$

$-1/2 \qquad 1/2$
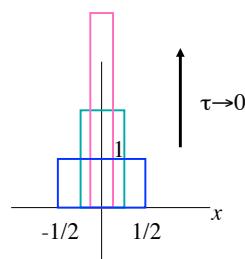
2D Dirac Delta Function

$\delta(x,y) = 0$ when $x^2 + y^2 \neq 0$ and $\int_{-\infty}^{\infty}\int_{-\infty}^{\infty}\delta(x,y)dxdy = 1$

where we can consider the limit of the integral of an ordinary 2D function that is shrinking in width but increasing in height while maintaining constant area.

$\int_{-\infty}^{\infty}\int_{-\infty}^{\infty}\delta(x,y)dxdy = \lim_{\tau \to 0}\int_{-\infty}^{\infty}\int_{-\infty}^{\infty}\tau^{-2}\Pi(x/\tau, y/\tau)dxdy$.

Useful fact : $\delta(x,y) = \delta(x)\delta(y)$


$\tau \to 0$
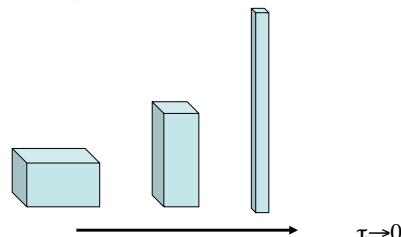
5

Generalized Functions

Dirac delta functions are not ordinary functions that are defined by their value at each point. Instead, they are generalized functions that are defined by what they do underneath an integral.

The most important property of the Dirac delta is the sifting property $\int_{-\infty}^{\infty} \delta(x - x_0) g(x) dx = g(x_0)$ where $g(x)$ is a smooth function. This sifting property can be understood by considering the limiting case

$$\lim_{\tau \to 0} \int_{-\infty}^{\infty} \tau^{-1} \Pi(x/\tau) g(x) dx = g(x_0)$$

g(x)

Area = (height)(width)= $(g(x_0)/\tau)\,\tau = g(x_0)$

x_0
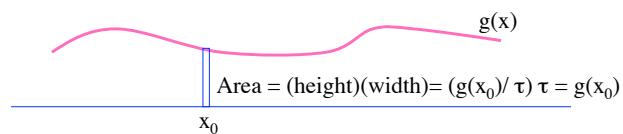
Representation of 1D Function

From the sifting property, we can write a 1D function as

$g(x) = \int_{-\infty}^{\infty} g(\xi) \delta(x - \xi) d\xi.$ To gain intuition, consider the approximation

$$g(x) \approx \sum_{n=-\infty}^{\infty} g(n\Delta x) \frac{1}{\Delta x} \Pi\left(\frac{x - n\Delta x}{\Delta x}\right) \Delta x.$$

g(x)
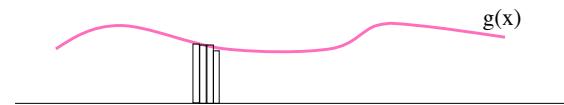
Representation of 2D Function

Similarly, we can write a 2D function as

$g(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} g(\xi,\eta) \delta(x - \xi, y - \eta) d\xi d\eta.$

To gain intuition, consider the approximation

$$g(x,y) \approx \sum_{m=-\infty}^{\infty} \sum_{n=-\infty}^{\infty} g(n\Delta x, m\Delta y) \frac{1}{\Delta x} \Pi\left(\frac{x - n\Delta x}{\Delta x}\right) \frac{1}{\Delta y} \Pi\left(\frac{y - m\Delta y}{\Delta y}\right) \Delta x \Delta y.$$
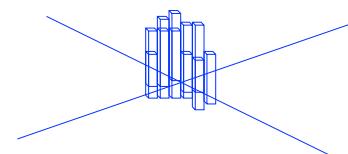
Impulse Response

Intuition: the impulse response is the response of a system to an input of infinitesimal width and unit area.

Original
Image

Blurred Image
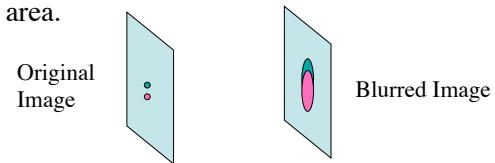
Since any input can be thought of as the weighted sum of impulses, a linear system is characterized by its impulse response(s).

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Impulse Response

The impulse response characterizes the response of a system over all space to a Dirac delta impulse function at a certain location.

$$h(x_2;\xi) = L\left[\delta(x_1 - \xi)\right] \qquad \text{1D Impulse Response}$$

$$h(x_2,y_2;\xi,\eta) = L\left[\delta(x_1 - \xi, y_1 - \eta)\right] \qquad \text{2D Impulse Response}$$
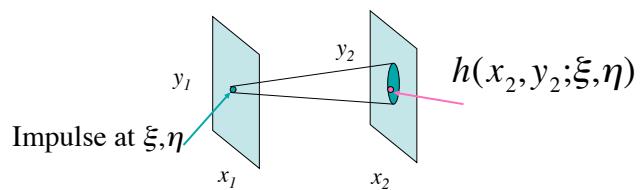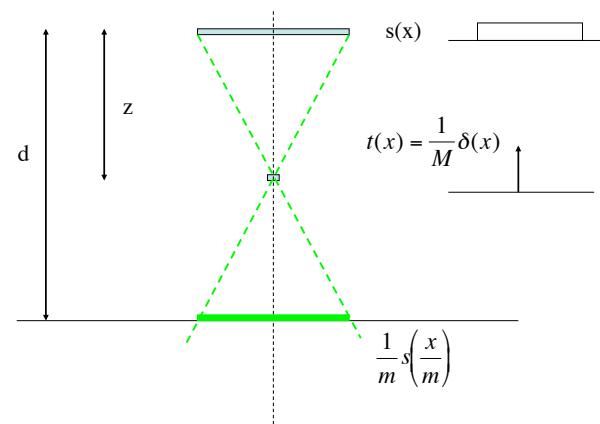
$$h(x_2, y_2;\xi,\eta)$$

Impulse at ξ,η

x_1 $\qquad$ x_2

y_1 $\qquad$ y_2

X-Ray Imaging

s(x)

z

d

$$t(x) = \frac{1}{M}\delta(x)$$

$$\frac{1}{m}s\left(\frac{x}{m}\right)$$

(A) Point Stimulus $\qquad$ (B) Isotropic PSF $\qquad$ (C) Non-Isotropic PSF

Contrasting Wire →

(D) Tomographic Image $\qquad$ (E) PSF

Bushberg et al 2001

$h(x - x_1)$ $\qquad$ $h(x - x_2)$

Separation

FWHM $\qquad$ FWHM

x_1 $\qquad$ x_2

(a)
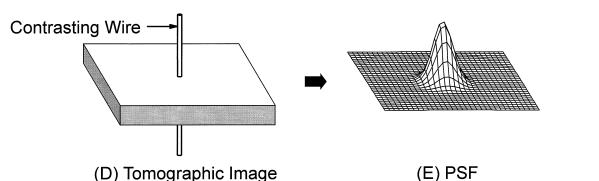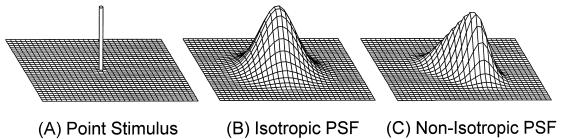
Full Width Half Maximum (FWHM) is a measure of resolution.

Separation

(b)

FWHM

Separation

(c)

Separation

(d)
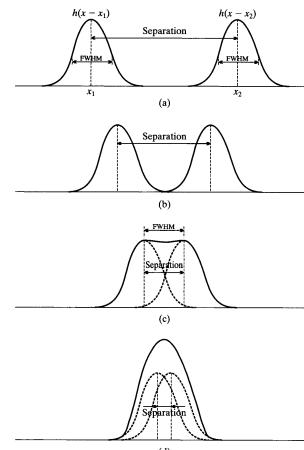
Figure 3.6
An example of the effect of system resolution on the ability to differentiate two points. The FWHM equals the minimum distance that the two points must be separated in order to be distinguishable.

Prince and Link 2005

Linearity (Addition)

$I_1(x,y)$ → R(I) → $K_1(x,y)$

$I_2(x,y)$ → R(I) → $K_2(x,y)$

$I_1(x,y) + I_2(x,y)$ → R(I) → $K_1(x,y) + K_2(x,y)$
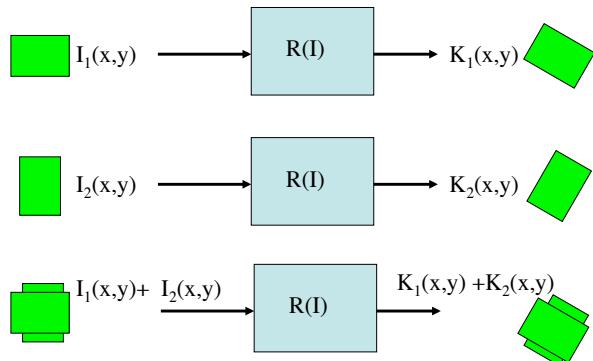
Linearity (Scaling)

$I_1(x,y)$ → R(I) → $K_1(x,y)$

$a_1 I_1(x,y)$ → R(I) → $a_1 K_1(x,y)$
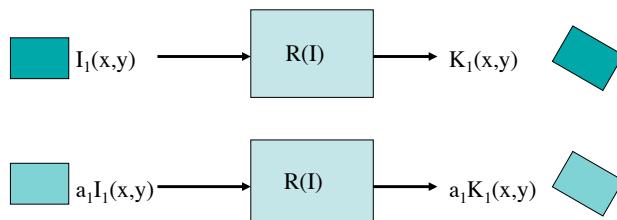
Linearity

A system R is linear if for two inputs
$I_1(x,y)$ and $I_2(x,y)$ with outputs

$R(I_1(x,y))=K_1(x,y)$ and $R(I_2(x,y))=K_2(x,y)$

the response to the weighted sum of inputs is the
weighted sum of outputs:

$R(a_1 I_1(x,y) + a_2 I_2(x,y)) = a_1 K_1(x,y) + a_2 K_2(x,y)$

Example

Are these linear systems?

(a) $g(x,y)$ → + → $g(x,y)+10$

10

(b) $g(x,y)$ → X → $10g(x,y)$

10

(c)

$g(x,y)$ → | Move up By 1 | → | Move right By 1 | → $g(x-1,y-1)$

pollEV.com/be280a

8
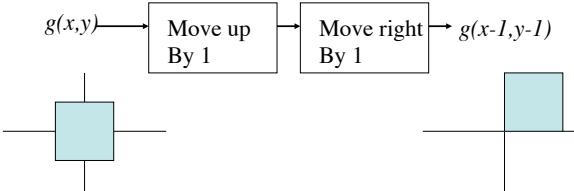
Superposition

$$g[m] = g[0]\delta[m] + g[1]\delta[m-1] + g[2]\delta[m-2]$$

$$h[m',k] = L[\delta[m-k]]$$

$$
\begin{aligned}
y[m'] &= L\big[g[m]\big] \\
&= L\big[g[0]\delta[m] + g[1]\delta[m-1] + g[2]\delta[m-2]\big] \\
&= L\big[g[0]\delta[m]\big] + L\big[g[1]\delta[m-1]\big] + L\big[g[2]\delta[m-2]\big] \\
&= g[0]L\big[\delta[m]\big] + g[1]L\big[\delta[m-1]\big] + g[2]L\big[\delta[m-2]\big] \\
&= g[0]h[m',0] + g[1]h[m',1] + g[2]h[m',2] \\
&= \sum_{k=0}^{2} g[k]h[m',k]
\end{aligned}
$$
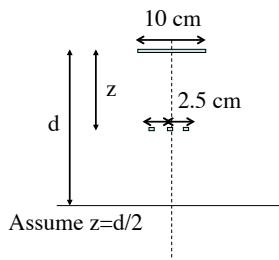
Superposition Integral

What is the response to an arbitrary function $g(x_1, y_1)$?

Write $g(x_1, y_1) = \int_{-\infty}^{\infty}\int_{-\infty}^{\infty} g(\xi,\eta)\delta(x_1 - \xi, y_1 - \eta)\,d\xi d\eta$.

The response is given by

$$
\begin{aligned}
I(x_2, y_2) &= L\big[g_1(x_1, y_1)\big] \\
&= L\Big[\int_{-\infty}^{\infty}\int_{-\infty}^{\infty} g(\xi,\eta)\delta(x_1 - \xi, y_1 - \eta)\,d\xi d\eta\Big] \\
&= \int_{-\infty}^{\infty}\int_{-\infty}^{\infty} g(\xi,\eta)L\big[\delta(x_1 - \xi, y_1 - \eta)\big]\,d\xi d\eta \\
&= \int_{-\infty}^{\infty}\int_{-\infty}^{\infty} g(\xi,\eta)h(x_2, y_2; \xi,\eta)\,d\xi d\eta
\end{aligned}
$$

Superposition Example

10 cm

z

2.5 cm

d

Assume z=d/2

Space Invariance

If a system is space invariant, the impulse response depends only on the difference between the output coordinates and the position of the impulse and is given by $h(x_2, y_2; \xi,\eta) = h(x_2 - \xi, y_2 - \eta)$
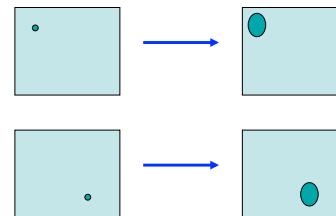
9

X-Ray Imaging

$s(x)$

$t(x) = \dfrac{1}{M}\delta(x)$

$\dfrac{1}{m}s\left(\dfrac{x}{m}\right)$

z

d

Is this a linear system?
Is it a space invariant system?

pollEV.com/be280a

---

10 cm

5 cm

z

d

Assume z=d/2

10 cm

5 cm

z

d

Assume z=d/2

10 cm

10 cm

z

d

Assume z=d/2
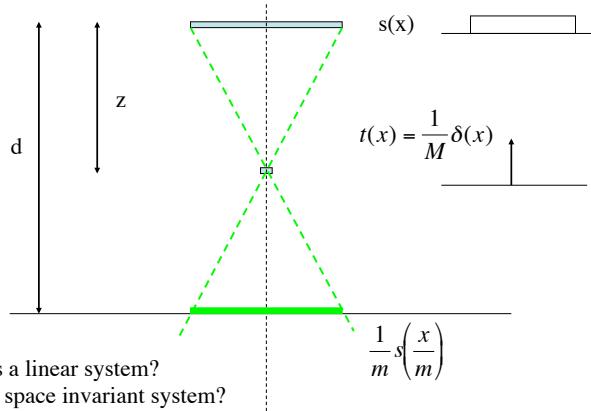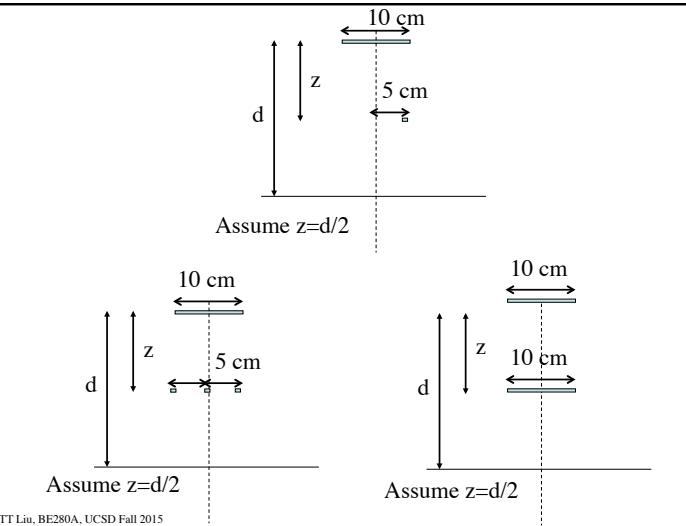
Convolution

$$g[m] = g[0]\delta[m] + g[1]\delta[m-1] + g[2]\delta[m-2]$$

$$h[m',k] = L[\delta[m-k]] = h[m'-k]$$

$$
\begin{aligned}
y[m'] &= L\big[g[m]\big] \\
&= L\big[g[0]\delta[m] + g[1]\delta[m-1] + g[2]\delta[m-2]\big] \\
&= L\big[g[0]\delta[m]\big] + L\big[g[1]\delta[m-1]\big] + L\big[g[2]\delta[m-2]\big] \\
&= g[0]L\big[\delta[m]\big] + g[1]L\big[\delta[m-1]\big] + g[2]L\big[\delta[m-2]\big] \\
&= g[0]h[m'-0] + g[1]h[m'-1] + g[2]h[m'-2] \\
&= \sum_{k=0}^{2} g[k]h[m'-k]
\end{aligned}
$$

1D Convolution

$$
\begin{aligned}
I(x) &= \int_{-\infty}^{\infty} g(\xi)h(x;\xi)d\xi \\
&= \int_{-\infty}^{\infty} g(\xi)h(x-\xi)d\xi \\
&= g(x) * h(x)
\end{aligned}
$$

Useful fact:

$$
\begin{aligned}
g(x) * \delta(x-\Delta) &= \int_{-\infty}^{\infty} g(\xi)\delta(x-\Delta-\xi)d\xi \\
&= g(x-\Delta)
\end{aligned}
$$

2D Convolution

For a space invariant linear system, the superposition integral becomes a convolution integral.

$$I(x_2, y_2) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} g(\xi, \eta) h(x_2, y_2; \xi, \eta) d\xi d\eta$$

$$= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} g(\xi, \eta) h(x_2 - \xi, y_2 - \eta) d\xi d\eta$$

$$= g(x_2, y_2) ** h(x_2, y_2)$$

where ** denotes 2D convolution. This will sometimes be abbreviated as *, e.g. $I(x_2, y_2) = g(x_2, y_2) * h(x_2, y_2)$.
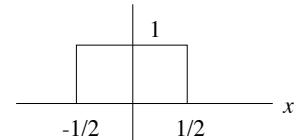
# Rectangle Function

$$\Pi(x) = \begin{cases} 0 & |x| > 1/2 \\ 1 & |x| \le 1/2 \end{cases}$$

Also called rect(x)

$$\Pi(x, y) = \Pi(x)\Pi(y)$$
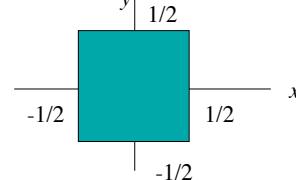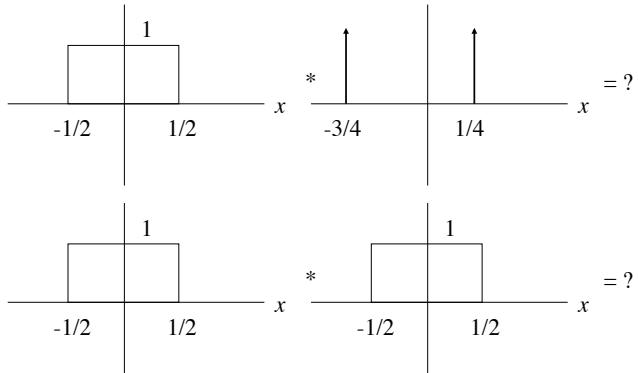
1D Convolution Examples

2D Convolution Example

$g(x) = \delta(x+1/2, y) + \delta(x, y)$ $h(x) = rect(x, y)$
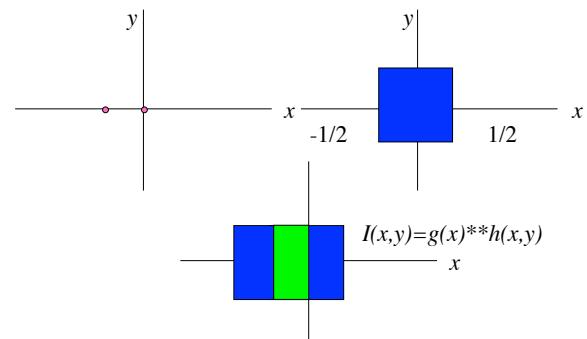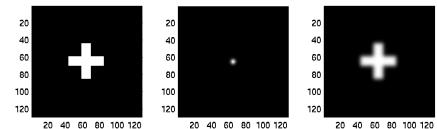
$I(x, y) = g(x) ** h(x, y)$

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2D Convolution Example

X-Ray Imaging

$$s(x)$$

$$t(x) = \frac{1}{M}\delta(x)$$

$$\frac{1}{m}s\left(\frac{x}{m}\right)$$

X-Ray Imaging

$$s(x)$$

$$t(x) = \frac{1}{M}\delta(x - x_0)$$

$$x_0$$

$$M(z) = \frac{d}{z}; \quad m(z) = -\frac{d-z}{z}$$

$$Mx_0 \qquad \frac{1}{m}s\left(\frac{x - Mx_0}{m}\right)$$
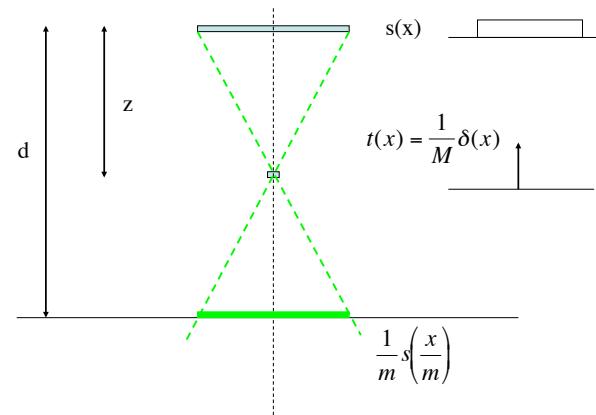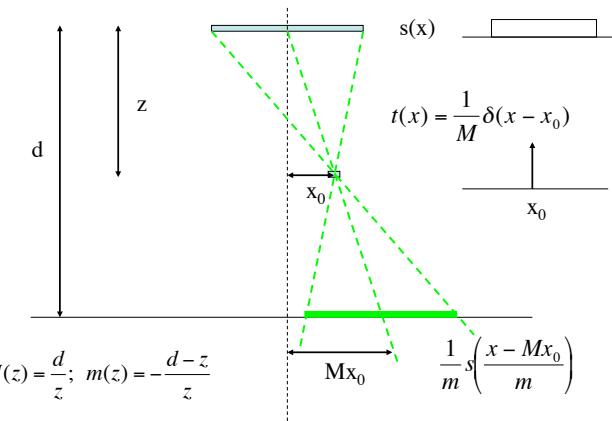
X-Ray Imaging

For off-center pinhole object, the shifted source image can be written as

$$s\left(\frac{x - Mx_0}{m}\right) = s\left(\frac{x}{m}\right) * \frac{1}{M}\delta\left(\frac{x - Mx_0}{M}\right)$$

$$= s(x/m) * t\left(\frac{x}{M}\right)$$

For the general 2D case, we convolve the magnified object with the impulse response

$$I(x,y) = t\left(\frac{x}{M}, \frac{y}{M}\right) ** \frac{1}{m^2}s\left(\frac{x}{m}, \frac{y}{m}\right)$$

Note: we have ignored obliquity factors etc.

X-Ray Imaging

$m = 1; M = 2$

$$\frac{1}{m} s\left(\frac{x}{m}\right) * t\left(\frac{x}{M}\right) = rect(x/10) * rect(x/20)$$

$$= ???$$

Field of view

Point source

Diaphragm

Object projection

(a)

Penumbra

Extended source

Penumbra

(b)

Edge blurring

Extended source

Edge blurring

Diaphragm

(c)
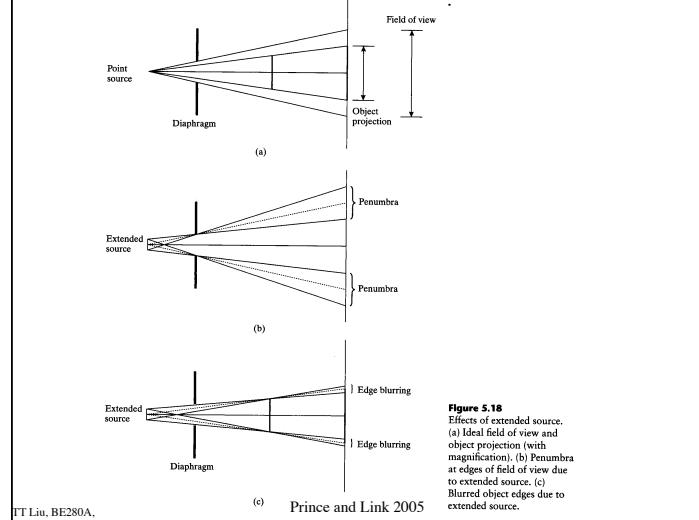
Figure 5.18
Effects of extended source. (a) Ideal field of view and object projection (with magnification). (b) Penumbra at edges of field of view due to extended source. (c) Blurred object edges due to extended source.

Prince and Link 2005

Summary

1. The response to a linear system can be characterized by a spatially varying impulse response and the application of the superposition integral.
2. A shift invariant linear system can be characterized by its impulse response and the application of a convolution integral.